Mechanoreceptor Activation in the Treatment of Drug-Use Disorders: Mechanism and Outcome

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Mechanoreceptor Activation in the Treatment of Drug-Use Disorders:
Mechanism and Outcome

Kyle Bills

A dissertation submitted to the faculty of
Brigham Young University
in partial fulfillment of the requirements for the degree of
Doctor of Philosophy

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ABSTRACT

Mechanoreceptor Activation in the Treatment of Drug-Use Disorders:
Mechanism and Outcome

Kyle Bills
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The therapeutic benefits attributed to activation of peripheral mechanoreceptors are poorly understood. There is growing evidence that mechanical stimulation modulates substrates in the supraspinal central nervous system (CNS) that are outside the canonical somatosensory circuits. This work demonstrates that activation of peripheral mechnoreceptors via mechanical stimulation (MStim) is sufficient to increase dopamine release in the nucleus accumbens (NAc), alter neuron firing rate in the ventral tegmental area (VTA) and increase membrane translocation of delta opioid receptors (DORs) in the NAc. Further, we demonstrate that these effects are dependent on DORs and acetylcholine receptors. Additionally, MStim can block neuronal markers of chronic ethanol dependence including ethanol-induced changes to VTA GABA neuron firing during withdrawal, and DA release profiles after reinstatement ethanol during withdrawal. These are presented in tandem with evidence that MStim also ameliorates behavioral indices of ethanol withdrawal. Finally, exercise, a modality that includes a mechanosensory component, is shown to alter expression of kappa opioid receptors (KORs) in the NAc. This change substantively depresses KORs influence over evoked DA release in direct contraversion to the effects of chronic ethanol. These changes translate into reduced drinking behavior.

Keywords: mechanoreceptors, dopamine, GABA, nucleus accumbens, ventral tegmental area, delta-opioid receptors, kappa-opioid receptors, exercise, alcohol, cholinergic interneurons, whole-body vibration
ACKNOWLEDGEMENTS

Thanks are owed first and foremost to God for the allowance of life, liberty and means to pursue greater understanding and outcome for those trapped in the grips of addiction. I am ever grateful for my wife Stephanie who, for reasons known only to her, has always shown great confidence in my ability to discharge the duties at hand. She is selfless, loving, thoughtful, beautiful and a myriad of other superlative things that cannot be listed in a reasonable volume. I owe much to my parents and sisters who cared for business interests during this educational sabbatical. I am thankful for the guidance and mentoring I received from Scott Steffensen, upon whom my training and support rested. Without his generosity and willingness to take risks on unproven theories, I would not have been able to perform these experiments. I could not have imagined a better man to work for. I offer my thanks to Jordan Yorgason, who was critical in my learning to perform experiments and reason as a scientist should. I am additionally grateful to Andrew Payne and Daniel Obray and James Brundage, wonderful colleagues who are kind, patient and wonderful examples of what I want to be. Finally, to countless undergraduate students without whom our laboratory would come to a halt.
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CHAPTER 1: Introduction

Scope of the Problem

Alcohol addiction is a chronic relapsing disease that affects more Americans than all forms of cancer combined (SAMHSA, 2016). It leads to destructive psychological, physical, social, and economic consequences. It is estimated that over 28 million Americans are currently in need of treatment for alcohol abuse, resulting in over $249 billion in direct costs (Sacks, Gonzales, Bouchery, Tomedi, & Brewer, 2015). Making matters worse, only 13% of those needing intervention actually receive it. Further, in spite of the wonderful advances in our understanding of the neuropathophysiology of addiction, the success rate of treatment has not substantively changed over the last hundred years, with around 50% of those treated relapsing (Moos & Moos, 2006; SAMHSA, 2016; White, 2012) within a year. This represents approximately 6% of those suffering from the disease receiving effective treatment. A report ranking the different conditions relative to the “global burden of disease” found that alcohol ranked 3rd out of the 25 major contributors (Lim et al., 2012). Developing new treatments looms seismically as a determinant quest for addiction researchers until, at the least, outcomes are markedly improved.

Mesolimbic Dopamine System and Dependence

The primary form of alcohol abused by humans is ethanol. It is clear that ethanol’s rewarding and addictive properties are mediated, in large part, by dopamine (DA)
neurotransmission in the mesolimbic system. Projections originate in the ventral tegmental area (VTA) of the midbrain and travel to the nucleus accumbens (NAc) in the ventral striatum (Fig. 1.1).

Dopamine release in the NAc represents a scalar index of reward (Wise, 2008), with increased levels associated with increased reward. Levels of DA increase with acute consumption of drugs of abuse, providing a reinforcing stimulus for further use (Carboni, Imperato, Perezzani, & Di Chiara, 1989; Yoshimoto, McBride, Lumeng, & Li, 1992). During the withdrawal state, neuroplastic alterations occur in the mesolimbic DA circuit leading to hypofunction (Karkhanis, Huggins, Rose, & Jones, 2016; Koeltzow & White, 2003; Maisonneuve, Ho, & Kreek, 1995; Rose et al., 2016). This reduction in DA is theorized to be the primary driver of relapse as blocking or ablating this pathway leads to dramatic decreases in drug self-administration (Lyness & Smith, 1992). Although the prevailing dogma is that DA neurons projecting from the VTA to the NAc mediate the rewarding and addictive properties of drugs of abuse (Wise, 2008), GABA neurons in the VTA have garnered much interest of late for their role in modulating DA release and as independent substrates mediating drug reward. Acute administration of cocaine, ethanol and methamphetamine have been shown to cause inhibition of VTA GABA neurons (Gallegos, Criado, Lee, Henriksen, & Steffensen, 1999; Ludlow et al., 2009; Steffensen et al., 2008;
Steffensen et al., 2009; Stobbs et al., 2004), producing a net disinhibition of VTA DA neurons (Bocklisch et al., 2013; Carboni et al., 1989; Yoshimoto et al., 1992). In contrast, in a state of withdrawal, VTA GABA neurons undergo plasticity and become hyperactive (Bonci & Williams, 1997; Gallegos et al., 1999; Hopf et al., 2007) leading to decreased mesolimbic DA release in the NAc (Karkhanis et al., 2016; Koeltzow & White, 2003; Maisonneuve et al., 1995; Rose et al., 2016). Understanding ethanol’s effects on the mesolimbic system is a singular challenge. This difficulty stems, in part, from the fact that there is no known ethanol receptor, rather a myriad of interactions between cell subtypes that change from acute to chronic exposure and again in the withdrawal state.

Dopamine Receptors

Two distinct sub classifications of DA receptors are commonly described. These are the D1 and D2 classes. Though the two families share a high degree of homology in their respective transmembrane domains, pharmacologically, they are distinct. D1 family receptors, including D1 and D5, are thought to be found on both pre- and postsynaptic membranes. In the ventral striatum they can be found on GABA-ergic medium spiny neurons (Beaulieu & Gainetdinov, 2011). These receptors are coupled to Gαs G-proteins which ultimately increase the likelihood of postsynaptic depolarization (Rankin & Sibley, 2010). The D2-like family of DA receptors include D2, D3, and D4 receptor subtypes. The D2 subtype can be broken down further into two
distinct isoforms, the long form (D2Lh) and the short form (D2Sh). There is currently much debate regarding their relative locations and contributions. It has been reported that the D2Sh subtype are predominately presynaptic, though this matter is not settled (Usiello et al., 2000). D2 receptors, broadly, are coupled to Gαi G-proteins. They cause a decrease in cAMP levels and subsequent reduction in DA release (Fig. 1.2). D2 receptors produce an auto-inhibitory feedback mechanism that is particularly important when studying ethanol, which acutely increases DA levels and D2 receptor activity, and chronically, decreases DA levels and D2 activity. Dopamine 2 receptors are reportedly in flux as the mesolimbic system progresses from acute ethanol exposure to a state of dependence. It is reported that ethanol preferring rats demonstrate a reduction in D2 receptor density (McBride, Chernet, Dyr, Lumeng, & Li, 1993; Stefanini et al., 1992; Strother, Lumeng, Li, & McBride, 2003). Further, ethanol preferring rats show a reduction in D2 receptor efficacy (Hietala et al., 1994). These receptors are expressed on cell bodies, dendrites and axons of cholinergic interneurons (CINs) in the NAc (Alcantara, Chen, Herring, Mendenhall, & Berlanga, 2003). Accumbal CINs activate nicotinic acetylcholine (ACh) receptors on DA terminals and increase DA neurotransmission (Yorgason, Zeppenfeld, & Williams, 2017).
Opioid Receptors

There are three well described classical opioid receptor (OR) types, kappa (KOR), mu (MOR), and delta (DOR). Others types have been described and debated (ORL1, sigma, epsilon, orphinan, etc…). We will focus on the three classical opioid receptors with implications to the mesolimbic DA system. These receptors are coupled to G_i-proteins and produce inhibition through several means, including inhibition of adenylate cyclase, reduction of calcium currents, and activation of inwardly rectifying potassium channels (Attali, Saya, & Vogel, 1989; Henry, Grandy, Lester, Davidson, & Chavkin, 1995; Konkoy & Childers, 1989; Prather et al., 1995; Tallent, Dichter, Bell, & Reisine, 1994). They also activate a number of kinase cascades such as the mitogen-activated protein kinase cascade (Fukuda, Kato, Morikawa, Shoda, & Mori, 1996). Many ligands activate these receptors with most cross-activating between the three; though they exhibit differing preferences. The main endogenous ligands involved in their activation are of three classes, dynorphins, which are derived from the precursor protein pro-dynorphin and are preferential for KORs (Aldrich & McLaughlin, 2009); enkephalins, which are derived from pro-opiomelanocortin and are preferential to MORs and DORs; and endorphins, which are also derived from pro-opiomelanocortin and have a preference for MORs. These receptors are similar in structure and have some overlap in ligand binding. Though activation of all receptor types is associated with analgesia, MORs and DORs produce euphoria and increased risk for dependence while KORs, conversely, when activated elicit dysphoria.

Kappa Opioid Receptors

KORs are expressed extensively in the NAc, both in the core and the shell (Mansour, Burke, Pavlic, Akil, & Watson, 1996; Mansour, Khachaturian, Lewis, Akil, & Watson, 1987; Spanagel, Herz, & Shippenberg, 1992), where their activation inhibits DA release (Spanagel et al., 1992). Data suggests that they are synthesized in the cell bodies of DA neurons in the VTA
where they are expressed and also subsequently transported to terminals in the NAc where they are integrated into the presynaptic membrane (Fig. 1.3) (Mansour, Fox, Akil, & Watson, 1995). Activation of KORs is associated with dysphoria (Shippenberg, Zapata, & Chefer, 2007). Evidence suggests that there is an upregulation of KORs in alcohol-dependent animals that may play a role in the increased seeking behavior seen with dependence (Sirohi, Bakalkin, & Walker, 2012). This is demonstrated by a decrease in dependent-state seeking behavior when the KOR antagonist nor-BNI is administered while having no effect on non-dependent animals (Walker & Koob, 2008). Further chronic intermittent ethanol exposure has been shown to increase the effect of KORs in the NAc. These data suggest a role for KORs in the synaptic adaptations that accrue to alcohol dependence (Shippenberg et al., 2007).

**Mu (MOR) and Delta (DOR) Opioid Receptors**

In contrast to KORs, MORs and DORs are associated with euphoria, imparting to agonists of these receptors a high potential for abuse (Devine & Wise, 1994). Activation facilitates DA release in the NAc by two mechanisms. First, MORs and DORs act on local GABA interneurons in the NAc increasing DA release, presumably, through disinhibition of DA terminals, cholinergic interneurons, and glutamatergic projections to the NAc.

![Fig 1.3: Location of mesolimbic opioid receptors](image)
(Fig. 1.3) (Hirose et al., 2005; Murakawa et al., 2004; Okutsu et al., 2006; Yoshida et al., 1999). Second, MORs on GABA interneurons in the VTA disinhibit DA projections to the NAc (Bonci & Williams, 1997; Johnson & North, 1992; Steffensen et al., 2006). Though some aspects of MOR and DOR activity is similar, there are profound differences in their respective contributions to ethanol dependence. Non-selective MOR and DOR antagonists have been shown to decrease ethanol’s enhancement of DA release in the NAc in rats (Acquas, Meloni, & Di Chiara, 1993; Benjamin, Grant, & Pohorecky, 1993; Lee et al., 2005). Interestingly, while mice that lack MORs, or have them selectively blocked, appear immune to the reinforcing effects of ethanol (Job et al., 2007; Roberts et al., 2000), those that lack DORs demonstrate an increase in ethanol seeking behavior (Roberts et al., 2001).

Recently, evidence has emerged implicating DORs in the mesolimbic effects of a targeted mechano-acupuncture treatment when given at the HT7 acupoint, located medial to the flexor carpi ulnaris tendon at the wrist. This mechanically-based treatment activates peripheral mechanoreceptors and excites the traditional somatosensory pathway from spine to nucleus cuneatus to thalamus (Chang et al., 2017). Interestingly, it has been shown to influence VTA GABA neurons, producing a transient inhibition in their firing and reducing ethanol-seeking behavior in rodents (Chang et al., 2017; Yang et al., 2010).

Mechanoreceptors as possible therapeutic targets for drug-use disorders

Previously, low and medium (2-100 hz) frequency electroacupuncture, which activates peripheral mechanoreceptors, has been shown to activate enkephalinergic and beta-endorphinergic neurons in the arcuate nucleus (Wang, Mao, & Han, 1990a, 1990b), which in turn inhibit GABA neurons, likely, via activation of mu- and delta-opioid receptors (MORs and DORs) (Mansour, Khachaturian, Lewis, Akil, & Watson, 1988; Yang et al., 2010). Further
acupuncture modulates VTA GABA neurons via somatosensory pathways and reduces ethanol and cocaine psychomotor effects and drug-seeking behavior (Chang et al., 2017; Jin et al., 2017; Kim et al., 2013; Yang et al., 2010; Yoon et al., 2012). Stimulation at HT7 (Shenmen acupoint) activates the dorsal column medial lemniscal (DCML) pathway, synapses in the nucleus cuneatus (CN) and subsequently relays through the thalamus and lateral habenula before finally modulating the excitability of VTA GABA neurons (Chang et al., 2017), presumably through DORs that are expressed on GABA neurons in the NAc core greater than the shell (Hipolito, Sanchez-Catalan, Zanolini, Polache, & Granero, 2008). We hypothesize that activation begins with peripheral mehcanoreceptors, such as Meissner’s, Pacinian corpuscles, and Merkel cells and ends wth DORs in the NAc. It is generally accepted that these receptors possess “optimal” frequency ranges in which they are most active. Merkel cells become more responsive with increased frequency and amplitude of stimulation in a near linear relationship from approximately 1-100 Hz and 1-1500 µm respectively (Rowe, Tracey, Mahns, Sahai, & Ivanusic, 2005). Meissner’s corpuscles are considered to become optimally activated at frequencies around 50 Hz (Macefield, 2005), while Pacinian corpuscles optimally respond to higher frequencies beginning as low as 100 Hz, but optimally in the range of 200-400 Hz (Biswas, Manivannan, & Srinivasan, 2015). The clarification of the neurological pathway underlying HT7’s mesolimbic effects suggests that activation of the pathway generally will be sufficient to produce the same effect.

*Scope of the Work Performed in This Dissertation*

To this point, several important factors underlying the use of mechanoreceptor stimulation in the treatment of drug abuse remain to be elucidated, including, determining whether mechanoreceptor activation alone is sufficient to alter mesolimbic function, critical
neuronal substrates activated, regional specificity of receptor activation, optimal vibrational frequency of mechanical stimulus, optimal duration of treatment and behavioral efficacy of the treatments in question. To this end, we originally proposed 2 specific aims to address these questions.

**Aim 1: To define the mechanism underlying the effects upon VTA GABA, DA neurons and NAc DA release elicited by subcutaneous vibration at the C7-T1 laminae and HT7.** The previously published literature combined with our preliminary data suggest that stimulation of the DCML neurological pathway will be sufficient to produce changes in the mesolimbic system. This aim sets out to show these effects, define the DCML and opioid receptors as mechanistically involved and describe the optimal vibrational frequency and duration for maximal effect. The **hypothesis** is that subcutaneous vibration will: 1) Produce a transient increase followed by a longer decrease in VTA GABA neuron firing rate and that vibration at HT7 and the C7-T1 laminae will produce the same changes; 2) Cause an increase in VTA DA neuron firing rate; 3) Increase evoked DA release in the NAc; 5) Exhibit a dose dependent response; and 6) Be reversed by ablation of the DCML or administration of naltrindole. These hypotheses will be tested with in vivo electrophysiology, and in situ NAc fast-scan cyclic voltammetry to evaluate phasic and spontaneous DA release, respectively.

**Aim 2: Evaluate the effects of subcutaneous vibration as an attenuator of cocaine psychomotor-activating effects, self-administration and ultrasonic vocalizations.**

Acute cocaine exposure has been shown to increase 50 KHz ultrasonic vocalizations and locomotor activity in rats. HT7 acupuncture has been shown to effectively decrease these psychomotor activities as well as self-administration. The **hypothesis** is that subcutaneous vibration or optogenetic stimulation will: 1) Decrease 50 KHz ultrasonic vocalizations and
locomotor activity in rats after acute cocaine exposure; 2) Decrease cocaine self-administration; and 3) Reduce the effects of acute cocaine exposure on VTA GABA and DA neurons and DA release in the NAc via their activation of DCML neurological pathway. These hypotheses will be tested with behavioral assays, in vivo electrophysiology, and voltammetry. Originally, the aims were narrowly focused on acupuncture as a modality. As our understanding increased, so did our scope, with expansion to mechanical stimulation of the cervical vertebrae at the C7-T1 level (MStim). After completing the studies outlined in Aim 1, it became clear that the effects elicited by MStim were robust and carried translational potential as a treatment for drug-use disorders. Our aims changed to accommodate a more complete understanding of the mechanistic nature of MStim-induced effects on the mesolimbic circuitry. In addition to the studies proposed we evaluated DA release in the NAc via microdialysis and pharmacologically studied the importance of DORs both systemically and locally in the VTA and NAc. Further, we looked at the importance of acetylcholine release in the NAc as a mediator of terminal DA release and the preeminence of the NAc as the mesolimbic entry point of MStim and the driver of VTA changes. Through immunohistological (IHC) methods, we examined the expression patterns of DORs in the VTA and NAc in response to MStim. These findings are described in Chapter 3. Aim 2 was changed substantively as well. Again, because of the translational potential of this treatment, we felt it more relevant to examine its effects on the withdrawal state rather than the acutely intoxicated state. Therefore, we studied MStim effects on chronic ethanol withdrawal. We examined VTA GABA neurons and DA release patterns in the NAc. We also measured behavioral metrics of withdrawal (Chapter 4). Finally, because of the broadened impact of MStim as opposed to acupuncture alone. We performed a study to investigate exercise induced alterations to chronic ethanol exposure. We examined these effects in the context of
KORs using fast-scan cyclic voltammetry and IHC staining. We also measured ethanol drinking behavior via a drink-in-the-dark paradigm (Chapter 5).

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doi:10.1016/j.neuropharm.2016.07.022


CHAPTER 2: Targeted Subcutaneous Vibration with Single-Neuron Electrophysiology as a Novel Method for Understanding the Central Effects of Peripheral Vibrational Therapy in a Rodent Model

Targeted Subcutaneous Vibration with Single-Neuron Electrophysiology as a Novel Method for Understanding the Central Effects of Peripheral Vibrational Therapy in a Rodent Model

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Abstract

Very little is known about the effects of whole body vibration on the supraspinal central nervous system. Though much clinical outcome data and mechanistic data about peripheral neural and musculoskeletal mechanisms have been explored, the lack of central understanding is a barrier to evidence-based, best practice guidelines in the use of vibrational therapy. Disparate methods of administration render study to study comparisons difficult. To address this lack of uniformity, we present the use of targeted subcutaneous vibration combined with simultaneous \textit{in vivo} electrophysiological recordings as a method of exploring the central effects of peripheral vibration therapy. We used implanted motors driven by both Grass stimulators and programmed micro controllers to vary frequency and location of stimulation in an anesthetized \textit{in vivo} rat model while simultaneously recording firing rate from GABA neurons in the ventral tegmental area. We show peripheral vibration can alter GABA neuron firing rate in a location and frequency dependent manner. We include detailed schematics and code to aid others in the replication of this technique. This method allows for control of previous weaknesses in the literature including variability in body position, vibrational intensity, node and anti-node interactions with areas of differing mechanoreceptor densities, and prefrontal cortex influence.
Introduction

Vibrational therapy, through the use of whole body vibration (WBV) platforms or localized peripheral vibration (LPV), is increasing in popularity. Early investigations looked at vibration-induced enhancement of physical performance such as power and strength\(^1\), and this body of literature is now extensive. Over the last 15 years, the vibration literature has rapidly expanded to include studies on a variety of responses ranging from flexibility\(^2,3\) and balance\(^4\), to bone metabolism\(^5\), hormone release\(^6\), and aging and loss of balance\(^7\). The application of vibration stimulates mechanoreceptors in the skin, muscle, and joint which influence monosynaptic and polysynaptic pathways in the peripheral and central nervous systems (PNS and CNS). Much of the initial explanation regarding the functional efficacy of WBV or LPV has focused on peripheral neuromechanical alterations.

Early work utilizing LPV directly to a tendon or muscle helped establish peripheral neuromechanical responses to vibration. Vibration can invoke the stretch reflex by exciting group Ia afferents\(^8\), while secondary afferents and Golgi tendon organs (GTO) show a decreased response to vibration input\(^9\). However, the firing rate of both afferents and the GTO response increase with muscle contraction\(^9,10\). Other studies suggest that both the H-reflex and stretch reflex are suppressed during vibration due to pre-synaptic inhibition\(^11\), and that this suppression is sustained following application of WBV\(^12,13\). Weight bearing activities and exercise application of WBV on reflex responses appears more controversial with load-bearing movement and complexity of tasks possibly interfering with assumed neuromechanisms\(^12\). More recently, however, the variability in results of similar studies and the broadening of vibration application for study has suggested a more important role of central or supraspinal influence. Reflex
contraction appears dependent on efferent fusimotor input, which suggests supraspinal control is involved\textsuperscript{14}. Current research observing the effects of vibration on symptoms of various medical conditions including stroke\textsuperscript{15} and Parkinson’s disease\textsuperscript{16}, amongst others\textsuperscript{17}, suggests that WBV is a safe and beneficial method for improving these symptoms, as well as general movement patterns, gait, and balance. Evaluation of such conditions offers further evidence that supraspinal and central mechanisms are involved in the body’s responses to vibration input. Reports of enhanced corticospinal excitability concomitant with spinal inhibition\textsuperscript{18} and facilitated motor evoked potentials\textsuperscript{19} further highlight the enhanced role of the central nervous system in modulating responses to vibration. The concomitant increased cortical excitability seems to compensate for lower excitability at the spinal level\textsuperscript{20}.

Touch (both fine and crude) pathways such as the dorsal column/medial lemniscal pathways (DCML) and pain/temperature pathways (anterolateral columns) are well defined in both texts and research literature regarding their structures and regions crossed as information is relayed from a peripheral receptor to the somatosensory cortex. However, activation of specific mechanoreceptor responses within a defined area and their effects on central neuron activity remains largely unknown. Mechanical stimulation of the DCML pathway via mechanoacupuncture at the wrist has been shown to produce modulatory effects in $\gamma$-aminobutyric acid (GABA)-containing neurons in the midbrain ventral tegmental area (VTA)\textsuperscript{21}. Further these effects have been traced through synapses in the nucleus cuneatus (CN) and subsequent relays through the thalamus and lateral habenula before finally producing inhibition of VTA GABA neurons\textsuperscript{21}. Thus, groundwork has been laid demonstrating, indirectly, that peripheral mechanoreceptor activation affects higher order functions of the CNS (e.g., limbic), beyond simple somatosensory processing. There is also
compelling evidence demonstrating central changes in response to mechanical vibration as measured with fMRI, EEG, heart rate variability and evoked potentials. Unfortunately, the lack of better detail to supraspinal responses is still an impediment to the development of evidence-based therapeutic guidelines and consensus on vibration’s therapeutic value and mechanism of action. The use of fMRI lacks temporal and spatial resolution and primarily gives regional specificity and indirect information about neuron activity. Conversely, the use of EEG offers improved temporal resolution but lacks regional specificity. Evoked potentials give information about a change in the facilitation/inhibition of the entire pathway with limitations similar to EEG. Heart rate variability also lacks spatiotemporal resolution and is, at best, a generalized indirect measure of autonomic nervous activity. These deficiencies underpin the need for novel methods of investigation to determine how peripheral mechanical vibration affects central activity. These previous methods leave a gap in the ability to understand how individual neurons within a targeted area respond to LPV.

In this paper, we lay out the application of localized subcutaneous vibration with simultaneous in-vivo single neuron electrophysiology. This technology has been a long-standing and commonly used technique to measure changes in neuron firing rate in response to various experimental conditions. However, to date, it has not been applied to the field of clinically applied vibration. Use of this technique can further our understanding of the non-canonical effects of LPV. Not only does this method give us the ability to understand the individual neuron response to LPV, but it also allows us to control the application of the peripheral vibration (region, frequency, and amplitude). To demonstrate the utility of this technique, we aimed to test regional and frequency-based differences in LPV on GABA neuron firing rate in the VTA. To test this, we implanted
subcutaneous vibrating motors in two different regions (posterior neck C7-T1 and the biceps femoris of the posterior hindlimb) of wistar rats. Further, we tested the difference between 50 Hz and 115 Hz at the C7-T1 level of the spinal column. We hypothesized that regional and frequency-based differences would produce disparate changes in GABA neuron firing rate due to differences in both mechanoreceptor density and specificity.

Materials and Methods

Vibrational Motors

The vibration excitation source used in this research was a 3 volt, DC coin vibration motor (10 mm x 2.7 mm, DC 3V/0.1A, Uxcell, Hong Kong, CN). This motor induces vibration due to a rotating unbalance. The motor is encased in a small circular disc with a 10 mm diameter and 2.7 mm length. The weight of the motor was 6 g. A photograph of the motor is shown in Figure 2.1.
To ensure proper excitation to the system through predictable output, the vibration output of the motor was evaluated. The procedure consisted of configuring the motor input voltage and then randomly selecting one of the predetermined frequencies. The motor output velocity was measured 10 times at each frequency and voltage setting using a laser Doppler vibrometer (LDV). The LDV provided a non-intrusive measurement without adding any mass to the motor. The displacement and acceleration were computed from the velocity measurements. Two input voltage settings of 1 volt and 2 volts were used. The frequencies tested were at every 10 Hz ranging from 40 Hz to 160 Hz.

The motor characterization results are shown in Figure 2.2. **Figure 2.2A** shows the amplitude of the motor output displacement as a function of frequency. The displacement data show a relatively flat frequency response from 80 Hz to 150 Hz. **Figure 2.2B** shows the acceleration versus frequency data for the motor. As expected, the acceleration output increases quadratically with frequency. From these data, it was determined that this motor had a fairly flat frequency response across the frequencies of interest and was sufficiently characterized to produce sufficiently repeatable results for the experiments described below.

*Surgical Procedure and In Vivo Single Cell Electrophysiology*
Wistar rats, weighing 250-320 g, from our breeding colony at Brigham Young University were used. Rats were housed in groups of 2-3 at a fixed temperature (21-23°C) and humidity (55-65%) on a reverse light/dark cycle with ad libitum food and water. Rats were anesthetized using isoflurane and placed in a stereotaxic apparatus. Anesthesia was then maintained at 1%. Body temperature was maintained at 37.4° ± 0.4°C by a feedback regulated heating pad. A 10 mm incision was made either at the C7-T1 levels posteriorly at midline or at the ipsilateral biceps femoris muscle. The Fascia was dissected and muscle tissue was left intact. A 10 mm x 2.7 mm, DC 3V/.1A micro coin vibration motor (Uxcell, Hong Kong, CN), was then implanted subcutaneously (to the right of midline for cervical implant) and the incision was closed adhesively. Extracellular potentials were recorded by a single 3.0 M KCl-filled micropipette (2 to 4 Mohms; 1-2 μm inside diameter). With the skull exposed, a hole was drilled for placement of the pipette which was driven into the VTA with a piezoelectric microdrive (EXFO Burleigh 8200 controller and Inchworm, Victor, NY) via stereotaxic coordinates [from bregma: 5.6 to 6.5 posterior (P), 0.5 to 1.0 lateral (L), 6.5 to 7.8 ventral (V)]. Potentials were displayed on a digital oscilloscope and amplified with an Axon Instruments Multiclamp 700A amplifier (Union City, CA). Single-cell activity was filtered at 0.3 to 10 kHz (3 dB) with Multiclamp 700A and sampled at 20 kHz (12 bit resolution) with National Instruments acquisition boards. Extracellularly recorded action potentials were discriminated with a WPI, WP-121 Spike Discriminator (Sarasota, FL). Single-unit potentials, discriminated spikes, and stimulation events were captured by National Instruments NB-MIO-16 digital I/O and counter/timer acquisition boards (Austin, TX) in Mac computers.

**Characterization of VTA GABA Neurons in vivo and Recordings**
VTA GABA neurons were identified by previously-established stereotaxic coordinates and by spontaneous and stimulus-evoked electrophysiological criteria. They included: relatively fast firing rate (>10Hz), ON-OFF phasic non-bursting activity, and spike duration less than 200 µsec. We evaluated only those spikes that had greater than 5:1 signal-to-noise ratio. After positive GABA neuron identification, baseline firing rate was measured for 5-minutes to ensure stability prior to vibratory stimulus.

_Grass Stimulator and Vibration Stimulation_
Following measurement of the GABA neuron baseline firing rate, a 60-second vibration stimulus was introduced. The vibrating motor was connected to the S44 Grass Stimulator (Grass Medical Instruments, West Warwick, RI). For electrophysiological recordings, the stimulator was set at 2 volts for 0.1 msec duration and 0 msec delay. Pulses per second were varied to produce variations in vibrational frequency. All vibratory stimuli were 60 sec in duration and followed by 15-min of recording the GABA neuron firing rate. Experimental groups included 50 Hz (n=4) and 115 Hz (n=4) given subcutaneously at the C7/T1 level and 50 Hz (n=4) given subcutaneously at the right biceps femoris muscle.

_Micro Controller Driver_
In order to facilitate the replication of this technique we include an alternative method for generating the vibratory stimulus using a PIC24F16KA301 micro controller to generate a pulse width modulation (PWM) signal. This PWM can be modified to emulate multiple signals of varying frequency and amplitude. The PWM is then passed through a transistor that provides the needed current to the motor. The full circuit is pictured in Figure 2.3 and the schematic and code to drive the micro controller can be found at http://github.com/steffensenlab.

Statistical Analysis

Single-unit, discriminated spikes were processed with IGOR Pro software (Wavemetrics, Lake Oswego, OR). Extracellularly recorded single-unit action potentials were discriminated by a peak detector digital processing LabVIEW algorithm. After 5-min of recording, the final 60 sec of firing rate data before vibrational stimulus were averaged to establish a baseline for comparison. The results for control, 50 Hz and 115 Hz vibrational groups were derived from calculations performed on ratemeter records and expressed as means ± SEM. All statistical tests were performed in JMP13. Data from each recording were normalized and combined and binned in 100 sec intervals for comparison across time. All comparisons were initially made using a one-way ANOVA. Following the ANOVA, all groups and bins were compared to corresponding controls using a Dunnett’s analysis. The control group was established by taking firing rate data from GABA neurons in rats that received no vibratory stimulation but did receive subcutaneous implants of
vibrating motors which were placed near the cervical spine as described previously. Baseline recordings (n=4) were normalized and combined prior to comparison with experimental groups. Figures were compiled using IGOR Pro Software.

Results

Figure 2.4 demonstrates the three LPV experimental conditions that were tested and compared to unstimulated baseline. Figure 2.4A shows stimulation at the right hind leg. A vibrational stimulus at this location of 50 Hz for 60 sec showed no significant change in GABA firing rate over any time frame. Figure 2.4B demonstrates the effects of a 115 Hz stimulation at C7-T1 for 60 sec. As with stimulation to the hind leg, 115 Hz did not show a change in GABA firing rate across any time. In contrast, Figure 2.4C reveals a depression in GABA neuron firing rate resultant from a 50 Hz vibration at C7-T1 for 60 sec. Initial ANOVA revealed differences between bins at 101-200 $[F_{3,11} = 16.7675, p=0.0002]$ and 201-300 sec $[F_{3,11} = 19.51, p = 0.0001]$. After 50 Hz stimulus was given at 100 sec, from time 100 to 200 sec, GABA neuron firing rate depressed to 48.3% (± 3.2%, n=4, p<.0001) of baseline and to 45.9% (± 7.3%,
n=4, \( p < .0001 \)) of baseline from 200 to 300 sec. No other time frame or experimental condition produced a significant change in firing rate.

**Figure 2.5A** shows group data comparing firing rate averages of all locations and frequencies from time of vibrational stimulus to 400 sec post-stimulation. Analysis revealed significant differences between average vibration-induced firing rate depression between groups \([F_{(3,11)} = 7.14 , \ p = 0.006]\). 50 Hz stimulation at the right C1-T1 laminae produced an average depression to 69.2\% (±3.0\%, n=4, \( p = 0.0002 \)) of baseline and was the only stimulus to produce a significant reduction in firing rate over time. Panel B compares the greatest firing rate depression produced in each experimental group. Because VTA GABA neurons exhibit a natural cyclical ebb and flow some variation is expected even within the unstimulated group. There was a significant difference between the minimum firing rates of the four experimental groups \([F_{(3,11)} = 7.8545 , \ p = 0.0044]\). Unstimulated baseline recordings produce a maximal drop to 78.1\% (± 0.4\%, n=4) of averaged baseline. All other maximal depressions were compared to the variation in the baseline group. 50 Hz vibration to the cervical spine produced an average maximal drop in firing rate to 24.8\% (±1.4\%, n=4, \( p = 0.003 \)) of baseline. No other group produced a significant inhibition to firing rate.
Discussion

These findings are suggestive that LPV produces transient changes to cellular excitability in the VTA. Further, that vibrational frequency and location of stimulus are important factors in peripheral vibration-induced changes. The sites of stimulation were chosen due to their disparate relative levels of mechanoreceptor expression in the subcutaneous tissue and adjacent joint capsules. In humans, high levels of cutaneous and joint mechanoreceptors have been identified in the intervertebral disc and facet joints of the spine, with greater relative levels in the cervical spine than thoracic or lumbar\textsuperscript{25,26}. The control stimulation was chosen due to its distance from joint mechanoreceptors. The motor implant site provided at least 20 mm of distance between the motor and the nearest joint. Further, there is a lack of cutaneous Pacinian corpuscle expression in rodents enhancing the effect of increased distance from joint \textsuperscript{27}. The two frequencies of vibration were chosen to more selectively activate either Meissner’s corpuscles or Pacinian corpuscles; the former having a lower intensity dynamic range of around 5-100 Hz and the latter a higher range of around 100-300 Hz \textsuperscript{28-31}. However, it is noted that these ranges are commonly thought to be approximate and some overlap certainly exists. A small population of lanceolate endings exist that have been shown to respond to vibration in a range around 5-200 Hz, though this population of endings has only been demonstrated in recordings of cat whisker hair \textsuperscript{32}. Other common cutaneous and joint mechanoreceptors are thought to be more specific to light touch (Merkel Cells) and stretch (Ruffini corpuscles) and thus are less likely to be significant in the presence of prolonged vibrational input \textsuperscript{33}. 50 and 115 Hz vibrational frequencies were chosen to more selectively target Meissner’s and Pacinian Corpuscles respectively.
VTA GABA neuron activity transiently and significantly decreased after targeted subcutaneous vibration at the C7-T1 level when stimulation occurred at 50 Hz. These changes were not present when stimulation was given at 115 Hz or when stimulation was given at the muscle belly of the biceps femoris muscle of the upper hind leg. Additionally, they suggest that targeted, anatomically-specific and frequency-variable vibration, coupled with single-unit extracellular electrophysiology is an effective method for measuring direct alterations in neuronal firing rate resultant from peripheral vibration. A previous study recording GABA neuron firing rate changes in the VTA due to acupuncture treatment suggested that receptor sensitivities might be responsible for the reported frequency dependent effects on these neurons. GABA neurons in the VTA were chosen due to internal preliminary data indicating their responsiveness to peripheral vibration and because of their relevance in addiction research. This method can be employed to further clarify regional and frequency based sensitivities, mechanoreceptors subtypes, and tractology involved in alterations of central neuronal function. To our knowledge this method has not been applied to the field of therapeutic vibration. It can provide a framework for ongoing description of the central pathways involved in this emerging field of physical medicine.

**Future Direction**

It is unknown the extent to which higher order neuronal processing affects the currently observed effects of WBV such as improvement in gait, movement patterns and balance. By extension, even less is understood about the changes that occur primarily in these higher circuits. This lack of understanding is a major impediment to our ability to develop optimized, evidence-based care protocols and could contribute to the mixed outcome data surrounding both WBV and LPV, and their therapeutic applications. The diversity of vibrational testing protocols divergent in
frequency, duration, type, amplitude, resonant location and subject positioning render inference about precise neural mechanisms difficult. The lack of homogenous testing protocols could contribute to the mixed reports of the efficacy of WBV in the treatment of various conditions. Indeed, it has been shown that slight variations in a subject’s posture or weight distribution can greatly affect the transmission of vibratory stimuli through the body. Future studies should focus on addressing these issues, specifically tracking the cellular and circuitry changes that contribute to current therapeutic applications and outcomes from WBV. Frequency and regional specificity along with duration or treatment must be addressed in order to maximize patient outcomes. These answers will be difficult to ascertain without directly measuring circuitry of interest in animal models and human subjects for each condition for which WBV is a potential therapy. An understanding of cellular and circuitry changes could provide insight into applications not currently being considered, including methods such as deep brain stimulation or genetic therapies. Localized subcutaneous vibration with simultaneous \textit{in vivo} single-unit electrophysiology can provide heretofore lacking information about individual neuronal changes in the central nervous system. Filling this gap may help provide a more complete picture of the central effects of vibratory therapeutics and lead to improved continuity of application and outcome in the future.

\textbf{Declaration of Conflicting Interests}  
The author(s) declared no potential conflicts of interest with respect to the research, authorship, and/or publication of this article.

\textbf{Funding}  
This work was supported by PHS NIH grants AA020919 and DA035958 to SCS.
References


Figure Legends

Figure 2.1: Vibrational motor

Figure 2.2: Motor displacement and acceleration by frequency
(A) Displacement. (B) Acceleration. The dots on the graphs represent an average of 10, test samples and the vertical lines at each data point represent one standard deviation above and below the indicated value.

Figure 2.3: Circuit for micro controller driving motor

Figure 2.4: Effects of variable frequency and locale subcutaneous vibrational stimulus on GABA neuron firing rate in the VTA
(A, B) 50Hz stim given at right hindleg (A) and 115 Hz stim given at cervical spine (B) show no effect on VTA GABA neuron firing rate. C- 50 Hz stim at cervical spine causes a 52.9% reduction in GABA firing rate from 100 to 300 sec.

Figure 2.5 Group data showing average and maximal GABA neuron firing rate depression from baseline
(A) 50 Hz stim to the cervical spine produces an average depression to 69.2% of baseline. (B) 50 Hz stim to the cervical spine produces an average maximal depression to 24.8% of baseline.
CHAPTER 3: Mechanical stimulation of cervical vertebrae modulates the discharge activity of ventral tegmental area neurons and dopamine release in the nucleus accumbens

Mechanical stimulation of cervical vertebrae modulates the discharge activity of ventral tegmental area neurons and dopamine release in the nucleus accumbens

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Running title: MStim Alters Neuronal Activity in VTA and NAc

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Number of pages: 32
Number of figures: 7
Abstract: 209 words
Introduction: 640 words
Discussion: 1412 words
Formatted for The Journal of Neuroscience
Abstract

The therapeutic benefits attributed to activation of peripheral mechanoreceptors are poorly understood. There is growing evidence that mechanical stimulation modulates substrates in the supraspinal central nervous system (CNS) that are outside the canonical somatosensory circuits. The aim of this study was to evaluate the effects of mechanical stimulation applied to the cervical spine at the C7-T1 level (termed “MStim”) on neurons and neurotransmitter release in the mesolimbic dopamine (DA) system, an area implicated in reward and motivation. Utilizing electrophysiological, pharmacological, neurochemical and immunohistochemical techniques in male Wistar rats we demonstrate that low frequency (45-80 Hz), but not higher frequency (115 Hz), MStim inhibited the firing rate of ventral tegmental area (VTA) GABA neurons (52.8% baseline; 450 sec) and concomitantly increased the firing rate of VTA DA neurons (248% baseline; 500 sec). Inactivation of the nucleus accumbens (NAc), or systemic or in situ antagonism of delta opioid receptors (DORs), blocked MStim inhibition of VTA GABA neuron firing rate. MStim enhanced both basal (178.4 % peak increase at 60 min) and evoked DA release in NAc (135.0 % peak increase at 40 min), which was blocked by in situ antagonism of DORs or acetylcholine release in the NAc. MStim enhanced the number of cells expressing c-FOS in the NAc, but inhibited total expression in the VTA, and induced translocation of DORs to neuronal membranes in the NAc. These findings suggest that MStim acts through endogenous opioids in the NAc to modulate DA release in the mesolimbic DA system. These findings demonstrate the need to explore more broadly the extra-somatosensory effects of peripheral mechanoreceptor activation and the specific role for mechanoreceptor-based therapies in the treatment of substance abuse.
Significance Statement

This research is the first to mechanistically describe a rationale for further exploration of physical medicine in the treatment of substance abuse. It is also the first to describe, mechanistically, robust and specific modulation of supraspinal brain circuits in response to targeted peripheral mechanical stimulation. It lays the groundwork for future studies to explore the effects of mechanical stimulation on other brain regions.
Introduction

The use of mechanoreceptor-based therapies in the treatment of drug-abuse disorders is a largely unexplored field. Indeed, the role of mechanoreceptors other than as canonical mediators of somato-sensation has only become relevant in recent years. Whole body vibration (WBV) has been shown to positively impact power and strength [1], flexibility [2, 3], balance [4], bone metabolism [5], hormone release [6], and falls in the elderly [7]. Notably, several complementary healthcare approaches are thought to have effects mediated in part by activation of mechanoreceptors, including chiropractic medicine, acupuncture, and physical therapy. Early understanding of the mechanisms underlying mechanoreceptor-based therapies such as WBV centered on peripheral neuromechanical alterations. Recent reports have included evidence of increased cortical excitability [8], increased motor evoked potentials [9], and compelling evidence demonstrating CNS changes in response to peripheral mechanical stimulation as measured with fMRI, EEG, heart rate variability, and evoked potentials [8, 10-12]. Notwithstanding these gains, our understanding of the CNS changes induced by peripheral mechanical stimulation remains understudied, and perhaps undervalued.

Midbrain dopamine (DA) neuron activity is involved in many aspects of reward seeking [13-15]. Although the prevailing dogma is that DA neurons mediate the rewarding and addictive properties of drugs of abuse [16], VTA GABA neurons have garnered much interest for their role in modulating DA neuronal activity and DA release and perhaps as independent substrates mediating reward or aversion [17-23]. We have shown previously that acute administration of ethanol, opioids, or cocaine inhibits VTA GABA neurons [17-21, 24], leading to a net disinhibition of VTA DA neurons [25-27]. In contrast, during ethanol or opioid withdrawal, VTA GABA neurons become hyperactive [17, 28] leading to decreased mesolimbic DA activity and release in the NAc [29-33]. This reduction in mesolimbic DA transmission is theorized to be the primary driver of relapse [34].

There is compelling evidence suggesting that some of the benefits ascribed to acupuncture are mediated through somatosensory neuronal pathways. We have shown in multiple reports that stimulation of the HT7 acupoint modifies drug-seeking behaviors and relapse to cocaine [35, 36], methamphetamine [37], and ethanol [38]. These effects can be attenuated with ablation of the dorsal column/medial lemniscal pathway and appear to act through endogenous opioids [39-41].
Though these studies demonstrate anatomically site-specific effects, they are suggestive that activation of primary somatosensory fibers generally may attenuate the reinforcing effects of drugs of abuse.

In this study, we hypothesized that mechanical stimulation of the cervical spine at C7-T1 (termed “MStim”) is sufficient to modulate neuronal activity in the VTA and neurotransmitter release in the NAc and that this effect is driven by activation of endogenous opioids. We have recently reported that MStim of the cervical spine modifies the activity of VTA GABA neurons [42]. Here we extend these studies to include the recording of VTA GABA and DA neurons, DA release, and mechanistic studies demonstrating the role of endogenous opioid release in mediating mechanoreceptor activation of the mesolimbic DA system.
Materials and Methods

Vibrational Motors
A 3 volt, DC coin vibration motor (10 mm x 2.7 mm, DC 3V/0.1A, Uxcell, Hong Kong, CN) was used as the source of vibrational stimulation. The motor, which was encased in a small circular disc with a 10 mm diameter and 2.7 mm width, created vibration due to off-centered weight attached to the motor’s rotational shaft. The weight of the motor was 1.5 g and its specifications and performance were as previously reported [42].

Animals and MStim Motor Implantation
Male wistar rats, weighing 250-320 g, from our breeding colony at Brigham Young University were used. Rats were housed in groups of 2-3 at 21-23°C and humidity (55-65%) on a reverse light/dark cycle with ad libitum food and water. A 10 mm incision was made either at the C7-T1 levels posteriorly at midline or at the ipsilateral biceps femoris muscle. The fascia was dissected and muscle tissue was left intact. A DC micro coin vibration motor was implanted subcutaneously (to the right of mid-line for cervical implant) and the incision was closed with surgical adhesive tape to maintain consistent motor placement.

Single Cell Electrophysiology
For recordings of VTA GABA neurons, rats were anesthetized using isoflurane and placed in a stereotaxic apparatus. Anesthesia was maintained at 1.5% with 2.0 L of air flow from a nebulizer (Isotec 4, Avante Charolette, NC) driven by an oxygen concentrator (Pureline, Nidek Gamagori Japan). For recordings of DA neurons, 1.5 g/kg urethane was injected IP. Body temperature was maintained at 37.4 ± 0.4°C by a feedback-regulated heating pad. With the skull exposed, a hole was drilled for placement of a 3.0 M KCl-filled micropipette (2 to 4 MΩ; 1-2 µm inside diameter), driven into the VTA with a piezoelectric microdrive (EXFO Burleigh 8200 controller and Inchworm, Victor, NY) based on stereotaxic coordinates [from bregma: 5.6 to 6.5 posterior (P), 0.5 to 1.0 lateral (L), 6.5 to 9.0 ventral (V)]. Potentials were amplified with an Multiclamp 700A amplifier (Axon Instruments, Molecular Devices, Union City, CA). Single-cell activity was filtered at 0.3 to 10 kHz (3 dB) with the Multiclamp 700A amplifier and displayed on Tektronix (Beaverton, OR) digital oscilloscopes. Potentials were sampled at 20 kHz (12 bit resolution) with National Instruments (Austin, TX) data acquisition boards in Macintosh computers (Apple
Computer, Cupertino, CA). Extracellularly recorded action potentials were discriminated with a World Precision Instruments WP-121 Spike Discriminator (Sarasota, FL) and converted to computer-level pulses. Single-unit potentials, discriminated spikes, and stimulation events were captured by National Instruments NB-MIO-16 digital I/O and counter/timer data acquisition boards in Macintosh computers.

**Characterization of VTA GABA and DA Neurons In vivo**

VTA GABA and DA neurons were identified by previously-established stereotaxic coordinates and by spontaneous electrophysiological and pharmacological criteria [43]. VTA GABA neuron discharge activity characteristics included: relatively fast firing rate (>10Hz), ON-OFF phasic non-bursting activity, and an initially negative spike with duration less than 200 µsec. In some experiments, GABA neurons were excited by DA (+40 nA) ejected iontophoretically from the recording pipette [20, 21, 44]. Dopamine neurons were identified by relatively slow firing rate (<10 Hz) and an initially positive-going spike of duration greater than 200 µsec. Most DA neurons were inhibited by iontophoretic DA from the recording pipette. We evaluated only those spikes that had greater than 5:1 signal-to-noise ratio. After positive neuron identification, baseline firing rate was measured for 5 min to ensure stability prior to MStim.

**Grass Stimulator and MStim for In-vivo Recordings**

Following measurement of neuronal baseline firing rate, a 60 or 120 sec MStim was introduced. The vibrating motor was controlled by a S44 Grass Stimulator (Grass Medical Instruments, West Warwick, RI). For electrophysiological recordings, the stimulator was set at 3 V for 0.1 msec duration and 0 msec delay [42]. Pulses/sec were varied to produce variations in vibrational frequency. All vibratory stimuli were 60 or 120 sec in duration and followed by 15 min of recording. Experimental groups included GABA neurons recordings following stimuli of 45, 80 and 115 Hz for both 60 and 120 sec with MStim given subcutaneously at the C7/T1 level, GABA neurons recordings following 80 Hz, 120 sec stimuli (this combination resulted in the greatest inhibition of GABA neuron firing rate and was used in all subsequent testing) given subcutaneously at the right biceps femoris muscle and DA neuron recordings after 80 Hz, 120 sec stimuli given subcutaneously at the C7/T1 level. Paired stimulation experiments were performed
with the second stimulation 60 sec after GABA neuron firing rate returned to baseline following the first stimulation.

**Fast-Scan Cyclic Voltammetry**

Evoked DA release in the NAc was measured by fast-scan cyclic voltammetry (FSCV) *in vivo*. A 7.0 μm diameter carbon fiber was inserted into borosilicate glass capillary tubing (1.2 mm o.d., A-M Systems, Sequim, WA, USA) under negative pressure and subsequently pulled on a vertical pipette puller (Narishige, East Meadow, NY, USA). The carbon fiber electrode (CFE) was cut under microscopic control with 150~200 μm of bare fiber protruding from the end of the glass micropipette. The CFE was back-filled with 3 M KCl. The electrode potential was linearly scanned with a triangular waveform from −0.4 V to 1.3 V and back to −0.4 V versus Ag/AgCl using a scan rate of 400 V/sec. Cyclic voltammograms were recorded at the CFE every 100 msec by means of a ChemClamp voltage clamp amplifier (Dagan Corporation, Minneapolis, MN, USA). Voltammetry recordings were performed and analyzed using customized software (Demon Voltammetry) [45]. For *in vivo* voltammetry recordings of DA signals, rats were anesthetized with 2% isoflurane and placed in a stereotaxic apparatus (David Kopf Instruments, Tujunga, CA, USA). Bipolar, coated stainless steel electrodes were stereotaxically implanted into the medial forebrain bundle (MFB; −2.5 mm posterior, +1.9 mm lateral from bregma, −8.0 to −8.3 mm from skull), and a capillary glass-based CFE in the NAc (+1.6 mm anterior, +1.9 mm lateral from bregma, −6.5 to −8.0 mm from skull). The MFB was stimulated with 60 monophasic pulses at 60 Hz (4 msec pulse width) at 2 min intervals until stable for five successive collections, defined as <10% variance. Recordings were performed in 2 min intervals, with baseline preceding the post-vibratory (80 Hz, 120 sec) recordings. Recordings were performed for 120 min or until baseline was reached, defined as 5 consecutive recordings at previously established baseline.

**Microdialysis and High Performance Liquid Chromatography**

Microdialysis probes (MD-2200, BASI) were stereotactically inserted into the NAc (+1.6 AP, +1.9 ML, −8.0 DV). Artificial cerebrospinal fluid (aCSF) composed of either 150 mM NaCl, 3 mM KCl, 1.4 mM CaCl₂, and 0.8 mM MgCl₂ in 10 mM phosphate buffer alone or, additionally, with either 10 nM naltrindole or a combination of 10 μM hexamethonium and 10 μM scopolamine was perfused through the probe at a rate of 3.0 μl/min. Samples were collected every 20 min for 4 hr
with MStim occurring after the first 2 hr had elapsed. Determination of the DA concentration in microdialysis samples was performed using a HPLC pump (Ultimate 3000, Dionex, Sunnyvale, CA, USA) connected to an electrochemical detector (Coulochem III, ESA). The detector included a guard cell (5020, ESA) set at +270 mV, a screen electrode (5014B, ESA) set at -100 mV, and a detection electrode (5014B, ESA) set at +220 mV. Dopamine was separated using a C18 reverse phase column (HR-80, Thermo Fisher Scientific, Waltham, MA, USA). Mobile phase containing 75 mM H₂NaO₄P, 1.7 mM sodium octane sulfonate, 25 µM EDTA, 0.714 mM triethylamine, and 10% acetonitrile was pumped through the system at a flow rate of 0.5 ml/min.

Preparation of Brain Slices for Imaging and Confocal Microscopy

Rats were anesthetized using isoflurane and placed in a stereotaxic apparatus. Anesthesia was maintained at 1.5% and motor was surgically implanted as described previously. MStim animals were given 120 sec of 80 Hz stimulation. Control animals had motors surgically implanted but not activated. After 2 hours animals underwent transcardial perfusion with 4% paraformaldehyde (PFA). Once perfused, brains were carefully removed and placed in 4% PFA for 24 hrs to facilitate continued fixation. After incubation in PFA, brains were placed in a solution of 30% sucrose in 1X PBS until the density of the brain matched that of the solution and the brains dropped to the bottom of the vial (~24-48 hrs). Brains were then flash frozen in dry ice and mounted on a cold microtome stage. Targeting the VTA and NAc, brains were sliced at 30 µm on the microtome and slices were placed in cryoprotectant (30% ethylene glycol, 30% sucrose, 0.00002% sodium azide, in 0.1 M PB) and kept at -20°C until staining. Slices were washed 3 times in 1x PBS for 10 minutes on a rotator. They were then blocked with a blocking buffer comprised of 4% normal goat serum, 0.1% Triton-X 100 and 1x PBS. Slices were then washed another 3 times in 0.2% PBST on a rotator. Primary antibodies were applied and allowed to incubate for 20 hours. Following staining the slices were washed 3 times in 0.2% PBST and secondary antibodies were applied. After a 2 hr incubation period they were washed another 3 times with 0.2% PBST and once with 1x PBS. Antibodies included Mouse anti-tyrosine hydroxylase (Novus, 1:1328), Sheep anti-c-FOS (Millipore, 1:1000) and Rabbit anti-DOR (LifeSpan, 1:200) as well as secondaries Alexa Fluor 405 Donkey Anti-Sheep from (1:900), Alexa Fluor 594 Goat anti-Rabbit (1:500). To mount slides, sections were placed on microscope slides and dried ~5 min. Once dried, a drop of vectashield (Vector Laboratories) was placed on the tissue, and a cover slip was placed on the slide. Slides set
overnight, and then they were kept at 4°C until imaging. An Olympus FluoView FV1000 confocal microscope was used to image mounted slices. Brain slices were mounted on microscope slides and imaged under oil immersion at 40X. To ensure consistent readings between samples, a constant photomultiplier tube voltage and gain were set between all acquired images.

Data Collection and Statistical Analysis

For single-unit electrophysiology studies, discriminated spikes were processed with a spike analyzer, digitized with National Instruments hardware and analyzed with National Instruments LabVIEW and IGOR Pro software (Wavemetrics, Lake Oswego, OR). Extracellularly recorded single-unit action potentials were discriminated by a peak detector digital processing LabVIEW algorithm. Firing rate data was averaged across neurons at 10 sec intervals and subsequently binned in 50 sec intervals for comparisons across time points. Experimental groups, in aggregate, were compared to unstimulated neurons using a one-way ANOVA then corresponding bins were compared with a Student’s t-test. Average depression or excitation in firing was calculated from the point where firing rate deviated by >10% from baseline to the time it returned to within 10% of baseline. Baseline firing rate was calculated from the average of the final 60 sec of firing rate data before vibrational stimulus and after 5 min of recording to ensure neuron stability. The results from all MStim and control groups were derived from calculations performed on ratemeter records and expressed as means ± SEM.

For microdialysis, the area under the curve for the DA peak was extracted and a two-point calibration was used to approximate the DA concentration. All collections were normalized to the final baseline collection before the MStim occurred. Standard error for the final baseline collection was approximated using the scalar property. Dopamine release for each timepoint following MStim was then compared to the baseline control using a Dunnett’s analysis. Reverse microdialysis and VTA injection experiments were compared to the MStim alone group using a Student’s t-test at the 60 min time point.

For FSCV, evoked recordings were normalized to the established baseline within subjects and then averaged across subjects in corresponding time intervals. Data was then binned in 10 min intervals. Comparisons were made for each 10 min bin to control using a Dunnett’s analysis. All
statistical tests were performed in JMP13 (SAS, Cary, NC). Figures were compiled using IGOR Pro Software (Wavemetrics, Lake Oswego, OR).

For brain slice imaging, images were loaded into FIJI software. Images were duplicated to preserve the original settings while color thresholding and brightness contrast adjustments were made to determine the location of cells and create ROIs. ROIs were then projected back onto the unedited images where area and mean intensity were recorded for each channel. This process was performed by three independent raters blinded to the hypothesis. To determine relative density of DORs, the ratio of mean fluorescence to area was determined.
Results

**MStim Modulation of VTA Neurons**

The effects of MStim on VTA GABA neuron firing rate were tested across multiple stimulus frequencies and durations (Fig. 3.1), as previously described[46]. MStim at 45 Hz (60 sec) significantly inhibited GABA neuron firing rate when compared to unstimulated baseline firing ($F_{(1,277)} = 24.9997, p<0.0001$; Fig. 3.1A). GABA neuron firing rate was significantly reduced from 50 sec to 250 sec post-stimulus when compared to baseline (n=4; 50 sec, $p=.0216$; 100 sec, $p=.0460$; 150 and 200 sec, $p<.0001$; 250 sec, $p=.0222$). Stimulation at 80 Hz (60 sec) ($F_{(1,272)} = 10.1423, p=0.0016$; Fig. 3.1B) produced GABA inhibition similar to that produced by 45 Hz, with significant depression from 100 to 250 sec post-stimulus (n=5; 100 sec, $p=.0186$; 150 and 200 sec, $p<.0001$; 250 sec, $p=.0101$). MStim effects with the same frequencies at a duration of 120 sec are shown in Fig. 3.1D-F. A 45 Hz stimulation (120 sec) significantly inhibited VTA GABA neurons ($F_{(1,282)} = 15.2029, p=0.0001$; Fig. 3.1D) similar to that observed with 60 sec MStim (n=5, 250 sec, $p=.0032$; 300 sec, $p<.0001$; 350 sec, $p=.0434$). The greatest inhibition to GABA neuron firing rate occurred following application of 80 Hz (120 sec) MStim ($F_{(1,296)} = 114.0478, p<0.0001$; Fig. 3.1E). Following this intervention, GABA neurons were significantly inhibited from 50 to 450 sec post-stimulus (n=7, 50-350 sec and 450 sec, $p<.0001$; 400 sec, $p=.0028$). In contrast, both 60 and 120 sec of 115 Hz stimulation (Fig. 3.1C,F) did not produce a significant depression to GABA neuron firing rate at any time point measured. Thus, GABA neuron firing was inhibited by MStim in a differential and frequency-dependent manner.

Somatosensory mechanoreceptor density varies by topographical location, with greatest density in the proximal joints and lower density in distal muscle [47, 48]. Therefore, to investigate differences in anatomical application of the MStim, a location with a relatively smaller concentration of mechanoreceptors was tested. Mechanical stimulation of 80 Hz (120 sec) at the belly of the right biceps femoris muscle produced only a small erratic decrease in GABA neuron firing rate when compared to the same stimulation at C7-T1 ($F_{(1,421)} = 146.4646, p<.0001$; Fig. 3.2A). The two were significantly different at 100-200 and 300 sec post-stimulus (n=4; 100 sec, $p=.0137$; 150 sec, $p=.0021$), suggesting that MStim-dependent inhibition of VTA GABA firing is greatest at areas of high mechanoreceptor density. Next, the effects of paired MStim was tested on VTA GABA firing rate (Fig. 3.2B). Compared to the second stimulation, the first typically produced greater inhibition of VTA GABA firing rate ($F_{(1,411)} = 29.2118, p<.0001$). Significant differences were
noted at 100-200 sec and 300 sec (n=5; 100 sec, p=.0137; 150 sec, p=.0021; 200 sec, 0.0078; 300 sec, p=.0033). Thus, MStim-dependent inhibition of firing rate was repeatable, but sensitive to desensitization-dependent processes. The 80 Hz (120 sec) stimulation produced the greatest effect on GABA neuron firing rate and was used in all subsequent experiments.

Since the dogma is that VTA GABA neurons provide inhibitory input onto local DA neurons, the effects of MStim on VTA DA neuron firing was tested. Dopamine neuron firing rate increased significantly post-stimulus ($F_{(1,429)} = 246.4261$, $p<0.0001$; Fig. 3.3A) reaching an average maximum increase of 286% of baseline at 150 sec post-stimulus. Firing rate increased significantly within the first 50 sec and stayed elevated to 500 sec post-stimulus. These time points (50-500 sec post-stimulus) were all significant when compared to unstimulated baseline DA neuron firing rate over time (n=5; 50-250 and 350-400 sec, $p<.0001$; 300 sec, $p=.0026$; 450 sec, $p=.0145$; 500 sec, $p=.0389$; Fig. 3.3B). On average, following MStim, DA neurons increased firing rate to 247% of baseline compared to 52.8 % inhibition observed in GABA neurons (Fig. 3.3C). The increase in DA neuron firing rate occurred in parallel to the reported decrease in GABA neuron firing rate noted from the same stimulation paradigm, suggesting disinhibition of DA neurons from decreased GABA neuron firing.

**MStim Modulation of VTA Neurons: Role of NAc Projections and Endogenous Opioids**

We have previously demonstrated that stimulation of the NAc inhibits VTA GABA neurons [43], via direct pathway GABAergic medium spiny neurons, and that opiate effects on VTA GABA neuron firing rate are mediated, in part, via GABA input to the VTA from the NAc [24]. To determine if MStim modulation of VTA GABA neurons was in the VTA or via NAc input to the VTA we evaluated the effects of in situ administration of the sodium channel blocker lidocaine into the NAc on MStim effects on VTA GABA neuron firing rate. Inactivation of NAc neurons by perfusion of lidocaine into the NAc via reverse microdialysis was sufficient to block MStim-induced depression of VTA GABA firing ($F_{(1,416)} = 246.9918$, $p<.0001$; n=5; Fig. 3.4A). All time points from 50-500 sec were significantly different (80 Hz 120 sec w/ lidocaine injection in NAc, n=5; 80 Hz 120 sec, n=7; 50 sec, $p<.0001$; 100 sec, $p<.0001$; 150 sec, $p<.0001$; 200 sec, $p<.0001$; 250 sec, $p<.0001$; 300 sec, $p<.0001$; 350 sec, $p=.0005$; 400 sec, $p<.0001$; 450 sec, $p<.0001$; 500 sec, $p<.0001$). We have previously shown that stimulation of the HT7 acupoint inhibits VTA GABA neuron firing rate, which is blocked by systemic administration of the non-selective opioid
receptor (OR) antagonist naloxone and the delta OR (DOR) antagonist naltrindole [38]. To better understand the role that DORs play in the underlying mechanisms responsible for the reported mesolimbic effects of MStim, the 80 Hz (120 sec) stimulation experiments were repeated while recording from GABA neurons in the VTA. First, systemic pretreatment with naltrindole (1 mg/kg IP), 15 min prior to MStim precluded the depression of GABA neuron firing rate \( F(1,487) = 190.4457, p < .0001; n=4; \text{Fig. 3.4A,B} \). The depression was blocked at every time point that was previously significant when comparing the 80 Hz stimulus to unstimulated baseline recordings in GABA neurons. The differences between 80 Hz w/ naltrindole and 80 Hz alone were pronounced and noted at all time points from 50-500 sec (80 Hz 120 sec w/ naltrindole, n=4; 80 Hz 120 sec, n=7; 50 sec, \( p < .0001 \); 100 sec, \( p < .0001 \); 150 sec, \( p < .0001 \); 200 sec, \( p < .0001 \); 250 sec, \( p < .0001 \); 300 sec, \( p < .0001 \); 350 sec, \( p = .0017 \); 400 sec, \( p = .0101 \); 450 sec, \( p = .0002 \); 500 sec, \( p < .0001 \)).

**MStim Enhancement of Dopamine Release: Role of Endogenous Opioids**

To determine if MStim-induced changes in DA firing might translate to an increase in DA neurotransmission, microdialysis and voltammetry experiments were performed on basal and evoked DA release in the NAc, respectively. Microdialysis experiments revealed an increase in basal release, with greatest release occurring from 40 – 60 min \( (178.43 \pm 26.24\% \text{ of baseline}), after \text{MStim} (n=15; 60 \text{ min, Dunnett’s, } p = .016; \text{Fig. 3.5A}) \). From 80 to 120 min post-stimulus, DA levels returned to baseline levels and stabilized. Next, voltammetry experiments were used to measure rapid changes in electrically evoked DA release. Evoked DA release rose slightly faster than basal release with significant increases 10 min post-stimulus (\text{Fig. 3.5B}). Increased levels of evoked DA release were significantly maintained from 10-50 min, peaking at 40 min \( (135.03 \pm 23.13\% \text{ of baseline}), with a return to baseline levels at 60 min (n=4; \text{Dunnett’s 10 min, } p = .0176; 20 \text{ min, } p = .0053; 30 \text{ min, } p = .0781; 40 \text{ min, } p = .0006; 50 \text{ min, } p = .0023) \). Thus, MStim produces increases in DA levels.

We then evaluated the role of endogenous opioids in mediating MStim-induced enhancement of DA release in the NAc. To determine the site specificity of the DORs involved in the effect (VTA versus NAc) we administered an ipsilateral injection of naltrindole into the VTA 15 min prior to stimulation and found unexpectedly that it did not attenuate MStim-induced DA release in the NAc \((n=15, \text{MStim alone}; n=4, \text{VTA naltrindole}; p = 0.570)\). Next, to determine whether local antagonism of NAc DORs contributes to MStim induced increases in DA release, we applied
naltrindole via reverse microdialysis (10 nM) in the NAc prior to MStim at the cervical spine (Fig. 3.6A). Local application of naltrindole blocked the MStim-induced increase in DA release in the NAc at the 60 min time point from 178.43 ± 26.24% of baseline in the MStim alone group to 88.0 ± 9.31% of baseline (n=15, MStim alone; n=8, naltrindole NAc; p=.0096; Fig. 3.6B). As sensory-driven cholinergic interneurons (CINs) in the NAc express DORs and have been shown to influence local DA release [49, 50], a combination of hexamethonium (10µM) and scopolamine (10µM) was then administered to the NAc via reverse microdialysis to evaluate the role of local acetylcholine (ACh) release on MStim induced DA release (Fig. 3.6A). At the 60 min time point DA release increased to 107.62 ± 3.4 % of baseline which represents significant attenuation of the MStim induced DA increase when compared to the MStim alone group (n=15, MStim alone; n=8, Hex/Scop NAc; p=.0311; Fig. 3.6B). These data suggest that the MStim-induced increase in DA release in the NAc is mediated through endogenous activation of DORs in the NAc and not the VTA and that the effect is in part influenced by local release of Ach from CINs.

**MStim Activation of NAc Neurons**

To further evaluate neuronal activation changes in the NAc and VTA and alterations in DOR expression in the NAc following MStim, post-MStim brain slices were stained to evaluate changes in relative expression of DORs and c-FOS. The number of cells per slide expressing DORs in the NAc was significantly increased in the MStim group when compared to control ($F_{(1,11)} = 10.6$, $p=0.008$; n=6; Fig. 3.7A,B,E). c-FOS expression in the NAc and VTA was analyzed for mean number of cell counts and mean fluorescent intensity (MFI). There was an increase in the number of cells expressing c-FOS in the NAc following MStim (53.0 ± 6.29) when compared to control (33.83 ± 6.79; $p=0.0314$, n=6), but not in the VTA (50.50 ± 2.94 vs 65.83 ± 9.36 cells; $p=0.0847$; Fig. 3.7C). However, when considering c-FOS MFI, there was a decrease in c-FOS expression in the VTA with MStim (109.6 ± 0.9% vs 116.8 ± 1.2%; $p=0.0071$, n=6; Fig. 3.7D), but not in the NAc. Together, these data suggest that the decrease in VTA c-FOS expression following MStim is likely due to enhanced inhibitory projections from the NAc.
Discussion

In this study, pathway specific experiments were performed to better understand the role of MStim in natural reward pathways. Low to high frequency (45-80 Hz) MStim produced robust inhibition of VTA GABA neurons. This was not surprising given our previous reports regarding mechanoreceptor-mediated inhibition of VTA GABA neurons [38, 42]. However, here we demonstrated that decreases in VTA GABA neuron firing by MStim are frequency, location, and time-dependent, and are accompanied by concomitant increases in VTA DA cell firing, increases in DA release in the NAc and mediation by endogenous opioid and local ACh release in the NAc.

The three frequencies tested were chosen to target specific mechanoreceptors. Of those chosen, 45 Hz enlists mostly Meissner’s corpuscles [51, 52], while 115 Hz is more selective for Pacinian corpuscles [53, 54]. Both receptors are subcutaneously located. The frequency of 80 Hz lies between the two and likely activates both receptors. Additionally, all three frequencies can activate Ruffini endings and Golgi tendon organs, two receptors that are morphologically similar to one another and are important as joint mechanoreceptors [55-57]. The 50 and 80 Hz MStim produced a transient depression of GABA neurons in the VTA, with 80 Hz (120 sec) producing the largest and longest lasting effect. Importantly, 80 Hz MStim failed to achieve a meaningful depression in VTA GABA neuron firing rate when applied at the belly of the biceps femoris muscle. This mid-muscle location was chosen because of its distance from joints and subsequent lower concentration of mechanoreceptors relative to the cervical spine [47, 48, 54].

Given that 80 Hz produced the greatest inhibition, 115 Hz failed to elicit a response and that the mid-muscle stimulation was ineffective at 80 Hz, suggesting a role for deep joint mechanoreceptors and Meissner’s corpuscle dependent pathways as main mediators of the resultant GABA depression. Taken together, these data suggest that the noted effects are only anatomically specific insomuch as anatomical location relates to the potential for mechanoreceptor recruitment. Even dorsal root ganglion cell bodies have been shown to depolarize in response to mechanical stimulation [58], perhaps enhancing the effects noted from stimulation to spine. It is also worth noting that subcutaneous stimulation provided in this study to the cervical spine is likely to have impacted most of the cervical and some of the thoracic spine, increasing the number of cutaneous and joint receptors activated. To our knowledge, this is the first evidence demonstrating that localized MStim increases DA neuron firing rate in the VTA and increases DA release in the NAc. Mechanical stimulation at 80 Hz (120 sec) elicited DA neuron firing of 247% baseline that occurred simultaneous to the average
depression of GABA neurons to 52.8% of baseline (Fig. 3.3C). This relationship suggests a disinhibition of DA neurons by way of GABA neuron depression.

Though previous studies have implicated DORs in the mechanoacupuncture-elicited depression of VTA GABA neurons [38], the location of DORs (spinal versus mesolimbic) has not been described. The present results suggest that mechanoreceptor stimulation results in increases in endogenous opioid release leading to transient modulation to the mesolimbic circuitry. There is a precedence for frequency-dependent release of endogenous opioids. For instance, in rats tolerant to morphine, low frequency (1-15 Hz) transcutaneous electrical nerve stimulation (TENS) was less effective than placebo controls at reducing joint inflammation, suggesting that TENS-alleviated joint inflammation is opioid dependent [59, 60]. Also, the effects of low frequency, but not high frequency, TENS stimulation are blocked by application of naloxone at doses selective for mu opioid receptors (MORs) and sparing of DORs and KORs [61]. Conversely, administration of the selective DOR antagonist naltrindole blocks the effects of high frequency TENS but spares those of a similar low frequency stimulation, though this effect appears to be isolated to spinal circuits [61]. While KORs have been shown on both cell bodies and terminals of DA neurons, MORs and DORs are absent [62]. However, DORs are located on synaptic terminals of GABA neurons in the VTA and NAc [62] and, of particular relevance to this study, on CINs in the NAc[63]. Delta opioid receptors are located in both the VTA and NAc [64, 65] and systemic (IP) administration of naltrindole blocked MStim effects on VTA neuron firing rate and DA release in the NAc. Interestingly, MStim-induced increase in NAc DA release was attenuated by selective blockade of DORs with naltrindole in the NAc but not the VTA. Corroboration of the VTA effects being driven by activity in the NAc was confirmed when MStim-induced VTA GABA neuron depression was blocked by local administration of lidocaine into the NAc. In light of the receptor distribution, the site-specific effect of DOR antagonists, the attenuation by NAc lidocaine application, the disparate expression of c-FOS in the NAc and VTA and the congruity of GABA depression and DA excitation (Fig. 3.4C), these data suggest that VTA effects are mainly due to NAc to VTA projections.

Voltammetry data shows a fast increase in evoked release that returns to baseline within 60 min while microdialysis shows a more gradual increase, peaking around 60 min post-stimulus (Fig. 3.5A and 3.5B). Interestingly, because GABA and DA neuron firing rates returned to baseline
after 464.3 and 366.7 sec post-stimulus, respectively, it is apparent that other factors influence the elevation in DA release, allowing release levels to remain elevated after VTA neuron firing rate has returned to baseline. This coupled with the fact that DA release was attenuated by blockade of both cholinergic and DORs in the NAc but not the VTA suggests that local factors related to DA terminals are the main drivers of MStim-induced DA release. One factor that needs careful consideration in the timing and mechanisms underlying MStim-induced DA increases are the multiple converging pathways onto the mesolimbic DA system (both in somatic and distal axonic regions). Dopamine terminals can be modulated independently of activity in cell body regions [49]. Specifically, sensory thalamic projections activate striatal CINs, which drive DA release through nicotinic acetylcholine (ACh) receptor activation. Further, accumbal DA release has been shown to increase with administration of DPDPE, a DOR agonist, in a dose-dependent manner with the effects lasting around 60 min in vivo when measured with microdialysis [66]. Therefore, it is also possible that MStim induces striatal release onto local DORs to further enhance DA release, as suggested by the near total blockage of MStim-induced DA release with NAc application of naltrindole. In the striatum, DORs exhibit increased levels of membrane translocation on CINs in response to acute cocaine administration, learning events and by activation of D1 receptors [67, 68]. This is particularly relevant considering the increased DOR translocation caused by MStim in the NAc. Activation of DORs on striatal CINs can induce hyperpolarization-activated currents that results in burst firing of CINs[67, 69], which can, in turn, lead to further release of DA by activation of ACh receptors located on DA terminals. As previously noted, MStim effects on VTA GABA neurons are likely secondary to MStim effects in the NAc and changes in DA release are likely through changes in CIN circuit effects, local activation of DORs and reciprocal projections from the NAc to VTA. It is also unknown if other non-GABA effects are contributing to MStim-induced increases in DA release.

Mechanoreceptors remain some of the least understood physiologic receptors, especially non-canonical activation effects on central processes including modulation of neurons in sub-cortical structures like the midbrain. Even some basic aspects of their methods of signal transduction and pathways recruited remain elusive. In spite of this, it is becoming increasingly evident that mechanoreceptors play a broader role than simply as somatosensory relay devices [1-4]. Here we begin exploration of their effects on mesolimbic circuitry. The mesolimbic DA system is a therapeutic target of treatments for a myriad of conditions including depression, ADHD, eating
disorders, Parkinson’s and addiction and there is a pressing need for new treatments to serve as adjuncts to current pharmacological approaches. Future studies should explore the possibility that practitioners of manual medicine, chiropractic physicians, acupuncturists, and physical therapists, might play in the development and implementation of adjunctive treatments for drug-abuse disorders. It remains to be seen if specific application of MStim therapy can alter drug-seeking behavior, which we are currently pursuing. Further, though these findings are specific to neurons in one circuit, they open the possibility that translational findings in other brain regions could lead to novel applications for mechanoreceptor-based therapies.
References


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Figure Legends

**Figure 3.1 – Frequency and duration-dependent effects of MStim on VTA GABA neuron firing rate.**

(A-C) Summarized time course data for 45 (A), 80 (B) and 115 Hz (C) stimulation at 60 sec duration. Representative ratemeter recordings of VTA GABA neurons are shown on the left and summarized data on the right. Note that 45 and 80 Hz MStim significantly inhibited the firing rate of VTA GABA neurons while 115 Hz had no effect. (D-F) The same set of frequency responses, but with a 120 sec stimulation. Note that 45 and 80 Hz MStim significantly inhibited VTA GABA neuron firing rate while 115 Hz had no effect, and that the inhibition was more pronounced with longer MStim durations. Asterisks *,**,*** indicate significance levels \( p<0.05, 0.01 \) and 0.001, respectively.

**Figure 3.2 – Spatiotemporal variation in MStim-induced effects on VTA GABA neuron firing rate.**

(A) VTA GABA neuron response to MStim (80 Hz; 120 sec) at the right biceps femoris muscle belly compared to cervical spine at C7-T1. Note that MStim at the biceps femoris was without effect on VTA GABA neuron firing rate. (B) VTA GABA neuron response to MStim at the C7-T1 vertebral level by two subsequent stimuli. Note the diminution in VTA GABA neuron firing rate with the second 80 Hz, 120 sec stimulation compared to the first. Asterisks *,**,*** indicate significance levels \( p<0.05, 0.01 \) and 0.001, respectively.

**Figure 3.3 – Dopamine neuron response to MStim.**

(A) Representative trace of DA neuron firing rate in response to MStim (80 Hz; 120 sec). Note that MStim markedly increased the firing rate of this VTA DA neuron. (B) Summarized time course comparing VTA DA neuron firing rate to MStim vs an unstimulated baseline. (C) Dopamine neuron firing rate changes compared to time-equivalent GABA neuron firing rate changes in response to MStim. (D) Summarized data comparing average firing rate changes in VTA neurons by MStim. Values in parentheses are n values. Asterisks *,**,*** indicate significance levels \( p<0.05, 0.01 \) and 0.001, respectively.
Figure 3.4 – Role of NAc inputs to the VTA and endogenous opioids in MStim-induced inhibition of VTA GABA neuron firing rate.

(A,B) Local injection of lidocaine into the NAc and IP administration of the DOR antagonist naltrindole blocked MStim-induced inhibition of VTA GABA neuron firing rate (80 Hz; 120 sec). Values in parentheses are n values. Asterisks *,**,*** indicate significance levels p<0.05, 0.01 and 0.001, respectively.

Figure 3.5 – MStim effects on basal and evoked DA release in the NAc.

(A) MStim enhanced basal DA release in the NAc, as measured by microdialysis. (B) Representative, superimposed voltammograms showing oxidation/reduction current vs voltage plots comparing DA release during baseline vs MStim. (C) Representative, superimposed current vs time plots showing DA release associated with local electrical stimulation. Calibration bars are nA and seconds. (D) MStim also enhanced evoked DA release in the NAc, as measured by voltammetry. Asterisks *,**,*** indicate significance levels p<0.05, 0.01 and 0.001, respectively.

Figure 3.6 – Role of DORs and CINs in MStim-induced enhancement of DA release in the NAc.

(A) Summarized time course of in situ NAc naltrindole or hexamethonium/scopolamine effects on MStim-induced enhancement of basal DA release in the NAc (80 Hz; 120 sec). Note that naltrindole or hexamethonium/scopolamine infusion into the NAc blocked MStim-induced enhancement of basal DA release. (B) Summarized data at the 60-min time point. Values in parentheses are n values. Asterisks *,**,*** indicate significance levels p<0.05, 0.01, and 0.001, respectively.

Figure 3.7 – MStim activates neurons and induces translocation of DORs in the NAc.

(A,B) Increased expression of DORs (red; TH is blue) in the NAc 2-hours post MStim compared to control. Insets show magnified views at point on 40X image indicated by the *. Note the translocation of DORs to the cell membrane. (C) Increased number of neurons in the NAc, but not the VTA, expressing c-FOS 2 hrs post MStim. (D) Decreased expression of c-FOS mean fluorescent intensity (MFI) in the VTA, but not in the NAc, 2 hrs post MStim. (E) Total number of NAc cells expressing DORs 2 hrs post MStim. Values in parentheses are n values. Asterisks *,** indicate significance levels p<0.05 and 0.01, respectively.
Figures

Figure 3.1

VTA GABA NEURONS

A  60 Sec/45 Hz

B  60 Sec/80 Hz

C  60 Sec/115 Hz

D  120 Sec/45 Hz

E  120 Sec/80 Hz

F  120 Sec/115 Hz
Figure 3.2

VTA GABA NEURONS

A

End Stim

Normalized Firing Rate

0.0
0.2
0.4
0.6
0.8
1.0
1.2
1.4

0 100 200 300 400 500

Seconds

Unstimulated
Femoris 80 Hz (120 sec)
C7-T1 80 Hz (120 sec)

B

End Stim

Normalized Firing Rate

0.4
0.6
0.8
1.0
1.2

0 100 200 300 400 500

Seconds

Unstimulated
1st 80 Hz
2nd 80 Hz

***

**

*
Figure 3.3

A. VTA DOPAMINE NEURONS

B. Normalized Firing Rate

C. DOPAMINE vs GABA NEURONS

D. Comparison of Normalized Firing Rate
Figure 3.4

(A) VTA GABA NEURONS

(B) Normalized Firing Rate

- Control
- 80 Hz
- Naltrindole (1 mg/kg IP)
- NAc Lidocaine
Figure 3.5

A. MICRODIALYSIS

B. VOLTAMMETRY

C. Stim

D. End Stim

Graph A shows the change in dopamine levels over time with the end of stimulation marked by an arrow. The y-axis represents dopamine concentration as a percentage of baseline, ranging from 80% to 220%. The x-axis represents time in minutes from 0 to 120.

Graph B depicts voltammetry results with arrows indicating baseline and 80 Hz conditions, showing potential changes in electric current at different voltage levels.

Graph C illustrates stimulation conditions, with an arrow indicating the moment of stimulation.

Graph D highlights the end of stimulation, with an arrow indicating the moment, and shows fluctuations in dopamine concentration with values expressed as a percentage of baseline.
Figure 3.6
Figure 3.7

(A) CONTROL

(B) MSTIM

(C) c-FOS CELL COUNT

(D) c-FOS MFI

(E) NAc DORs

(6) (6) (6) (6) (6) (6) (6)

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Mechanical stimulation alters chronic ethanol-induced changes to VTA GABA neurons, NAc DA release and measures of withdrawal

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Running title: MStim Alters Neuronal and Behavioral Effects of Chronic Ethanol

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Number of pages: 22
Number of figures: 3
Abstract: 132 words
Introduction: 768 words
Discussion: 572 words
Formatted for The Journal of Neuroscience
Abstract
Mechanical stimulation (MStim) has been previously shown to modulate firing rate of neurons in the ventral tegmental area (VTA) and dopamine (DA) release in the nucleus accumbens (NAc), an area of interest in alcohol-use disorder (AUD). In this study we examine the effects of MStim, during chronic alcohol dependence, on neurons in VTA and NAc and behavioral measures during withdrawal. We show that when MStim is administered concurrently with alcohol, it alters alcohol-induced desensitization of VTA GABA neuron firing rate in response to a reinstatement dose from 117.5% of baseline to 32.3%. Dopamine release in the NAc at 120 min post-injection is changed from 119.8% of baseline to 70.1%. Further, behavioral indices of withdrawal (rearing, open-field crosses, tail stiffness and gait) were substantively ameliorated with treatment with MStim.
Introduction

Alcohol addiction is a chronic relapsing disease that affects more Americans than all forms of cancer combined (SAMHSA, 2016). It leads to destructive psychological, physical, social, and economic consequences. It is estimated that over 28 million Americans are currently in need of treatment for alcohol abuse, resulting in over $249 billion in direct costs (Sacks et al., 2015). Making matters worse, only 13% of those needing intervention actually receive it. Further, in spite of the wonderful advances in our understanding of the neuropathophysiology of addiction, the success rate of treatment has not substantively changed over the last hundred years, with around 50% of those treated relapsing (Moos and Moos, 2006; White, 2012; SAMHSA, 2016). This represents approximately 6% of those suffering from the disease receiving effective treatment. A report ranking the different conditions relative to the “global burden of disease” found that ethanol ranked 3rd out of the 25 major contributors (Lim et al., 2012).

The current FDA-approved treatments for AUD are the sensitizing agent disulfiram, the mu-opioid receptor (MOR) antagonist naltrexone, and the neuromodulatory balancing agent acamprosate (Akbar et al., 2018). Many consider these pharmacological treatments to be woefully inadequate, and the public is begging for more efficacious treatments for AUD. Many are seeking alternative, non-invasive, non-pharmacological alternatives as personalized care and as adjuncts to self-help programs. Thus, more fundamental science and novel methods are needed to determine mechanisms underlying alternative approaches and improve outcomes.

The use of mechanoreceptor-based therapies (MStim) in the treatment of drug-abuse disorders is a largely unexplored field. Notably, several complementary health care approaches are thought to have effects mediated in part by activation of mechanoreceptors, including chiropractic medicine,
acupuncture, and physical therapy. There is compelling evidence suggesting that some of the benefits ascribed to acupuncture are mediated, through somatosensory neuronal pathways shared with MStim. We have shown in multiple reports that stimulation of the HT7 acupoint modifies drug-seeking behaviors and relapse to cocaine (Yoon et al., 2012; Jin et al., 2018), methamphetamine (Kim et al., 2019), and ethanol (Yang et al., 2010). These effects can be attenuated with ablation of the dorsal column/medial lemniscal pathway and appear to act through endogenous opioids (Yang et al., 2008; Kim et al., 2013; Chang et al., 2017). Though these studies demonstrate anatomically site-specific effects, they are suggestive that activation of primary somatosensory fibers generally may attenuate the reinforcing effects of drugs of abuse.

We have previously reported that MStim at 80 Hz to the cervical spine inhibits VTA GABA neuron firing, enhances VTA DA neuron firing and increases DA release in the NAc. Further, we have shown that VTA effects are driven by cholinergic interneurons (CIN) and delta opioid receptors (DOR) in the NAc. These findings are salient considering the role that the mesolimbic circuitry plays in reward, dependence and withdrawal. Midbrain dopamine (DA) neuron activity is involved in many aspects of reward seeking (Dalle Grave et al., 2008; Ranaldi, 2014; Gentry et al., 2018). Although the prevailing dogma is that DA neurons mediate the rewarding and addictive properties of drugs of abuse (Wise, 2008), VTA GABA neurons have garnered much interest for their role in modulating DA release and perhaps as independent substrates mediating reward or aversion (Gallegos et al., 1999; Stobbs et al., 2004; Steffensen et al., 2008; Ludlow et al., 2009; Steffensen et al., 2009; Brown et al., 2012; Tan et al., 2012). We have shown previously that acute administration of ethanol, opioids, or cocaine inhibits VTA GABA neurons (Gallegos et al., 1999; Stobbs et al., 2004; Steffensen et al., 2006; Steffensen et al., 2008; Ludlow et al., 2009; Steffensen et al., 2009), leading to a net disinhibition of VTA DA neurons (Carboni et al., 1989; Yoshimoto
et al., 1992; Bocklisch et al., 2013). In contrast, during ethanol or opioid withdrawal, VTA GABA neurons become hyperactive (Bonci and Williams, 1997; Gallegos et al., 1999) leading to decreased mesolimbic DA activity and release in the NAc (Maisonneuve et al., 1995; Koeltzow and White, 2003; Wise, 2004; Karkhanis et al., 2016; Rose et al., 2016). This reduction in mesolimbic DA transmission is theorized to be the primary driver of relapse (Lyness and Smith, 1992).

In this study, we investigate the role of MStim as a potential treatment for ethanol-use disorder by evaluating its ability to ameliorate chronic ethanol-induced changes to VTA GABA neuron firing, DA release in the NAc and behavioral indices related to withdrawal. We hypothesized that MStim is sufficient to block chronic ethanol-induced desensitization of VTA GABA neurons and changes in NAc DA release in response to ethanol reinstatement. Further, that MStim would block anxiety-related behaviors normally associated with chronic ethanol withdrawal.

Materials and Methods

Animals and MStim Motor Implantation
Male wistar rats, weighing 250-320 g, from our breeding colony at Brigham Young University were used. Rats were housed in groups of 2-3 at a fixed temperature (21-23°C) and humidity (55-65%) on a reverse light/dark cycle with ad libitum food and water. Rats were briefly anesthetized using isoflurane (4.0%) during injections to mitigate injection stress. Each received BID IP injections (9 am and 5 pm) of ethanol (2.5g/Kg; 16% w/v) or saline for 14-days. Intoxication was verified visually by noting loss of consciousness following initial injections with increasing tolerance. Immediately following injections MStim rats were placed on a LabWorks Inc ET-126
shaker device (Alpine, UT) with a sheet of 1/4 inch, 18 in x 18 in plexiglass fastened atop for 15-min. An 80 Hz, 500 mVpp sine wave was generated using a Wavetex Datron Universal Waveform Generator model 195 (San Diego, CA) and amplified using a Crown model XLi 3500 (Los Angeles, CA) amplifier. All animal received a final injection at 9am and were tested at 9am the following day. Experimental protocols were approved by the Brigham Young University Institutional Animal Care and Use Committee according to NIH guidelines.

**Single Cell Electrophysiology**

For recordings of VTA GABA neurons, rats were anesthetized using isoflurane and placed in a stereotaxic apparatus. Anesthesia was maintained at 1.5% with 2.0 L of air flow from a nebulizer driven by an oxygen concentrator. Body temperature was maintained at 37.4 ± 0.4°C by a feedback regulated heating pad. With the skull exposed, a hole was drilled for placement of a 3.0 M KCl-filled micropipette (2 to 4 MΩ; 1-2 µm inside diameter), driven into the VTA with a piezoelectric microdrive (EXFO Burleigh 8200 controller and Inchworm, Victor, NY) based on stereotaxic coordinates [from bregma: 5.6 to 6.5 posterior (P), 0.5 to 1.0 lateral (L), 6.5 to 9.0 ventral (V)]. Potentials were amplified with an Axon Instruments Multiclamp 700A amplifier (Union City, CA). Single-cell activity was filtered at 0.3 to 10 kHz (3 dB) with the Multiclamp 700A amplifier and displayed on Tektronix (Beaverton, OR) digital oscilloscopes. Potentials were sampled at 20 kHz (12 bit resolution) with National Instruments (Austin, TX) data acquisition boards in Macintosh computers (Apple Computer, Cupertino, CA). Extracellularly recorded action potentials were discriminated with a World Precision Instruments WP-121 Spike Discriminator (Sarasota, FL) and converted to computer-level pulses. Single-unit potentials, discriminated spikes, and stimulation events were captured by National Instruments NB-MIO-16 digital I/O and counter/timer data acquisition boards in Macintosh computers.
Characterization of VTA GABA

VTA GABA neurons were identified by previously-established stereotaxic coordinates and by spontaneous electrophysiological and pharmacological criteria (Steffensen et al., 1998). VTA GABA neuron discharge activity characteristics included: relatively fast firing rate (>10 Hz), ON-OFF phasic non-bursting activity, and an initially negative spike with duration less than 200 µsec. GABA neurons were excited by iontophoretic DA (+40 nA) ejected from the recording pipette. We evaluated only those spikes that had greater than 5:1 signal-to-noise ratio. After positive neuron identification, baseline firing rate was measured for 5 min to ensure stability prior to MStim.

Grass Stimulator and MStim for in-vivo Recordings

Following measurement of neuronal baseline firing rate, a 60 or 120 sec MStim was introduced. The vibrating motor was controlled by a S44 Grass Stimulator (Grass Medical Instruments, West Warwick, RI). For electrophysiological recordings, the stimulator was set at 3 V for 0.1 msec duration, 0 msec delay and 80 pulses/sec (Bills et al., 2019). All vibratory stimuli were 120 sec in duration and followed by 60 min of recording.

Microdialysis and High Performance Liquid Chromatography

Microdialysis probes (MD-2200, BASI) were stereotactically inserted into the NAc (+1.6 AP, +1.9 ML, -8.0 DV). Artificial cerebrospinal fluid (aCSF) composed of 150 mM NaCl, 3 mM KCl, 1.4 mM CaCl₂, and 0.8 mM MgCl₂ in 10 mM phosphate buffer was perfused through the probe at a rate of 3.0 µl/min. Samples were collected every 20 min for 4 hr with MStim occurring after the first 2 hr had elapsed. Determination of the DA concentration in microdialysis samples was
performed using a HPLC pump (Ultimate 3000, Dionex, Sunnyvale, CA, USA) connected to an
electrochemical detector (Coulochem III, ESA). The detector included a guard cell (5020, ESA)
set at +270 mV, a screen electrode (5014B, ESA) set at -100 mV, and a detection electrode (5014B,
ESA) set at +220 mV. Dopamine was separated using a C18 reverse phase column (HR-80,
Thermo Fisher Scientific, Waltham, MA, USA). Mobile phase containing 75 mM H2NaO4P, 1.7
mM sodium octane sulfonate, 25 μM EDTA, 0.714 mM triethylamine, and 10% acetonitrile was
pumped through the system at a flow rate of 0.5 ml/min.

Behavioral Measures of Withdrawal
Behavioral experiments were performed in a 16 T × 16 W × 32 L inch light attenuating plexiglass
compartment and were recorded using a camera mounted on the ceiling above the apparatus
connected to a Windows 7 PC running Pinnacle Studio 16 (Corel, Menlo Park, CA, USA). On
test days, withdrawal rats were placed in the center of the chamber and visually inspected and
subjectively scored for gait and tail stiffness. Each rat was scored twice by different raters blinded
to the rat’s experimental condition to reduce bias. The two scores were averaged. Tail stiffness
was scored 1-5 (1-no stiffness; 2-minor stiffness with no tail elevation with ambulation; 3-minor
stiffness with elevation during ambulation; 4-moderate stiffness with elevation at rest; 5- severe
stiffness with elevation at all times). Gait was scored 1-5 (1-normal movement pattern with no
hunching at rest or during ambulation; 2-normal movement patterns with mild hunching at rest but
not during ambulation; 3-abnormal movement patterns with mild hunching at rest but not during
ambulation; 4-abnormal movement patterns with moderate to severe hunching at rest but not suring
ambulation; 5-abnormal movement patterns with severe hunching at rest and during ambulation).
Open-field crosses were defined as the number of times the animal crossed through the middle 1/3
of the chamber and rears were defined as independent instances of both front paws leaving the ground and being elevated above resting head level.

*Data Collection and Statistical Analysis*

For single-unit electrophysiology studies, discriminated spikes were processed with a spike analyzer, digitized with National Instruments hardware and analyzed with National Instruments LabVIEW and IGOR Pro software (Wavemetrics, Lake Oswego, OR). Extracellularly recorded single-unit action potentials were discriminated by a peak detector digital processing LabVIEW algorithm and recorded in 10 sec intervals. Firing rate data was averaged across neurons at 10 sec intervals and subsequently binned in 50 sec intervals for comparisons across time points as previously reported (Bills, 2019). Experimental groups were averaged across bins and then compared using a one-way ANOVA then corresponding bins were compared with a Student’s t-test. Average depression or excitation in firing was calculated from 10-40 min post injection. Baseline firing rate was calculated from the average of the final 60 sec of firing rate data before vibrational stimulus and after 5 min of recording to ensure neuron stability. The results from all MStim and control groups were derived from calculations performed on ratemeter records and expressed as means ± SEM.

For microdialysis, the area under the curve for the DA peak was extracted and a two-point calibration was used to approximate the DA concentration. All collections were normalized to the final baseline collection before injection occurred. Standard error for the final baseline collection was approximated using the scalar property. Dopamine release for each time point was expressed as a percentages of baseline ± SEM. They were compared using a one-way ANOVA after which the groups were compared using a Tukey’s posthoc analysis.
For behavioral experiments, after blinded scoring, results were compared using a one-way ANOVA after which groups were compared using a Tukey’s posthoc analysis.

Results

Amelioration of chronic ethanol-induced changes to VTA GABA neurons by MStim

The effects of concurrent administration of 80 Hz MStim during chronic EtOH exposure were tested on VTA GABA neuron firing rate in the context of a reinstatement dose of EtOH (2.5g/kg IP) (Fig. 4.1). Baseline firing rate of GABA neurons in animals chronically exposed to EtOH was significantly higher (49.59 Hz) than that of animals that received concurrent MStim or saline with MStim (30.02 Hz and 35.94 Hz respectively) ($F_{(2,11)} = 5.1149, p=0.0269; \text{ Fig. 4.1D}$). Mechanical stimulation produced altered GABA neuron response to reinstatement EtOH when compared to chronic EtOH and saline groups ($F_{(2,108)} = 1348.799, p<0.0001; \text{ Fig. 4.1E}$)

Administration of 2.5g/kg IP reinstatement dose of EtOH in chronically exposed animals produced a slight increase in average GABA neuron firing to 117.52% ($±0.039, n=5$) of baseline. The same injection in MStim treated animals caused a decrease in firing to 32.72% ($±0.043, n=5$) of baseline while in saline treated rats it produced a drop to 14.71% ($±0.050, n=5$) of baseline. All groups were significantly different from each other (EtOH and MStim, p<0.0001; EtOH and Sal, p<0.0001; Sal and MStim, p<0.0001; \text{ Fig. 4.1F}). between MStim and saline groups (p=0.046). Thus, MStim, when given concurrently with chronic intermittent EtOH exposure to 2.5g/kg EtOH, blocks chronic EtOH-induced desensitization of VTA GABA neurons to reinstatement exposure.

MStim effects on chronic ethanol-induced changes to NAc DA release
To determine if blockage of chronic EtOH-induced changes to VTA GABA neuron firing rate by MStim translates to alterations in DA release in the NAc, dialysate samples were collected by microdialysis canula before and after a reinstatement dose of EtOH was given to rats after 24 hours of withdrawal (Fig. 4.2). Groups tested included a group naïve to both MStim and EtOH, EtOH, EtOH with MStim and saline with MStim. Animals naïve to both EtOH and MStim exhibited a rise in DA levels from 20 min to 120 min post-injection and significant differences were noted between the groups at those times (20 min, $F_{(3,13)} = 6.0631$, $p=0.0082$; 40 min, $F_{(3,13)} = 3.4890$, $p=0.0471$; 60 min, $F_{(3,13)} = 3.8812$, $p=0.0368$; 80 min, $F_{(3,13)} = 5.0333$, $p=0.0157$; 100 min, $F_{(3,13)} = 7.8089$, $p=0.0023$; 120 min, $F_{(3,13)} = 5.5628$, $p=0.0091$; Fig. 4.2A). Specific differences between groups were noted at min 20 between naïve and MStim groups (naïve n=8, MStim n=3, $p=0.0345$), at min 100 between naïve and MStim and naïve and saline groups (naïve n=8, MStim n=3, $p=0.0071$; saline n=3, $p=0.0147$) and at min 120 between naïve and saline groups ($p=0.0135$). Initial responses to ethanol reinstatement was uniform between the three experimentally exposed groups with DA levels demonstrating parity from minutes 20-80. At 100 minutes post-injection the EtOH group diverged from the other two measuring 95.42 % (±4.78) of baseline, closer to the naïve group which measured 119.99 % (±8.77). At this same timepoint the MStim and saline groups measured 57.61 % (±11.48) and 66.89 % (±16.78) respectively (Fig. 4.2B). At 120 min post-injection dopamine levels in the EtOH group elevated past baseline levels to 120.27 % (±10.28), which was in-line with the naïve response at 113.36 % (±5.91). Mechanostim and saline groups remained lower at 69.48 % (±13.16) and 47.90 % (±11.11) respectively. This is suggestive that MStim treatment alters DA release in response to ethanol in both previously exposed and unexposed animals.
**MStim blocks withdrawal symptoms in rats exposed to chronic EtOH**

To assess the behavioral relevance of MStim on indices of chronic EtOH withdrawal, rats in active withdrawal (24 hours after last dose) were evaluated for open field crosses, rearing behavior, tail stiffness and gait patterns (**Fig. 4.3**). Over a 30 min period, rats were assessed for the number of times they engaged in rearing. Mechanical stimulation ameliorated the reduction in rearing that was noted by chronic EtOH exposure alone \( (F_{(2,18)} = 14.8194, p=0.0002; \textbf{Fig. 4.3A}) \). The chronic EtOH rats engaged in rearing on average 22.57 times (±4.51). This was significantly fewer times than rats treated with concurrent MStim (n=8 in all groups; p=0.0011 for EtOH and MStim; p=0.0003 for EtOH and Sal). Mstim treated rats reared 46.29 times (±3.29) while saline treated rats reared 49.86 times (±3.65). Open-field crosses were defined as the number of times the rats crossed through the center 1/3 of the chamber in 30 min; it was also assessed. Mechanical stimulation blunted the Chronic EtOH-induced reduction in the number of times rats engaged in open-field crosses \( (F_{(2,18)} = 18.8606, p<0.0001; \textbf{Fig. 4.3B}) \). The chronic EtOH rats crossed 14.14 times (± 1.94). This was significantly fewer than the 29.86 (±1.77) and 31.14 (±2.71) crosses engaged in by the MStim and saline groups respectively (n=8 in all groups; p=0.0002 for EtOH and MStim; p<0.0001 for EtOH and Sal; **Figs. 4.3E-G**). Tail stiffness and gait were subjectively scored by two blinded assessors as further indicators of withdrawal status. Tail stiffness was increased in the chronic EtOH when compared to the MStim or saline groups \( (F_{(2,18)} = 36.1579, p<0.0001; \textbf{Fig. 4.3C}) \). Tail stiffness in the chronic EtOH group was significantly different from the other two and was scored 3.57/5 (±0.202) while the MStim and saline groups scored 1.86/5 (±0.261) and 1.14 (±0.143) respectively (n=8 in all groups; p<0.0001 for EtOH and MStim; p<0.0001 for EtOH and Sal). Differences in gait patterns were noted between the three groups \( (F_{(2,18)} = 13.5789, p=0.0003; \textbf{Fig. 4.3D}) \). Gait scores for chronic EtOH animals were 3.43/5 (±0.369). The MStim animals scored 1.71/5 (±0.184) and the saline group scored 1.43 (±0.297).
Chronic EtOH was significantly different from the other two (n=8 in all groups; p=0.0004 for EtOH and MStim; p=0.0017 for EtOH and Sal). Thus, MStim, when applied concurrently with chronic intermittent EtOH, is sufficient to ameliorate certain behavioral indices associated with chronic EtOH withdrawal.

Discussion

We have previously reported that MStim acts on the nucleus accumbens to increase local DA release and that this effect is mediated by activation of cholinergic and delta opioid receptors. Further, projections from the NAc then cause a depression in VTA GABA neuron firing which results in VTA DA neuron disinhibition and a subsequent increase in firing. The current study was designed to investigate if these neuromodulatory changes are sufficient to alter chronic ethanol effects on VTA GABA neurons and withdrawal behavior. In the present study, the effects of 80 Hz MStim treatment for 15 min BID given in-line with dependence-inducing chronic intermittent EtOH injections were tested on various measures of EtOH withdrawal. While acute administration of ethanol reduces VTA GABA neuron firing, chronic intermittent EtOH exposure desensitizes VTA GABA neurons during reinstatement doses (Gallegos et al., 1999). These effects are thought to occur through downregulation of D2 receptors in the VTA presumably due to EtOH-induced alterations in local VTA DA release (Ludlow et al., 2009). Concurrent administration of MStim with chronic intermittent EtOH blocks these effects and changes VTA GABA neuron response to reinstatement from 117.5% of baseline to 32.7% of baseline. The blunting of the desensitization was not sufficient to return the GABA neuron response back to a naïve state as there were significant differences between the saline group and the EtOH + MStim groups. Mechanical stimulation has been previously shown to increase DA levels in the NAc for 2 hrs post-MStim.
These increased levels activate D1 and D2 expressing medium spiny neurons in the NAc that project back to the VTA and target non-dopaminergic neurons (Xia et al., 2011). These projections could be responsible for MStim-induced changes in VTA GABA neurons response to chronic ethanol. These findings are particularly relevant as they represent a non-invasive method of blocking chronic ethanol effects.

Dopamine levels were tested in the same chronic reinstatement paradigm. Animals naïve demonstrated a characteristic increase in DA levels (Yim and Gonzales, 2000) following ethanol injection. Animals treated with EtOH alone or MStim, whether in conjunction with EtOH or not, did not exhibit the same increase in DA levels following EtOH administration. This is suggestive that MStim alone is sufficient to alter mechanistic changes normally elicited by the EtOH. Chronic EtOH administration has been shown to increase expression levels of DORs while decreasing expression of mu opioid receptors (Saland et al., 2005). As noted, we have previously shown that MStim produces increased translocation of DORs to cellular membranes, this commonality between EtOH and MStim could explain the desensitizing effects of MStim on acute EtOH administration in EtOH naïve rodents. The MStim-induced alterations to chronic ethanol effects on VTA GABA neurons and DA release in the NAc ultimately manifest in blunting of the noted markers of dependence. The behavioral studies reported here buoy that finding as all measures of withdrawal gathered for this study were substantively improved by the addition of MStim to the chronic intermittent EtOH exposure paradigm employed to induce dependence. These data, when taken as a whole suggest that MStim at 80 Hz could be a viable treatment option for the treatment of alcohol-use disorder (AUD). This study is practically limited by the fact that MStim exposure was given concurrently with EtOH exposure. It is less likely that individuals battling with AUD
will receive MStim at the time of first exposure to alcohol. Future studies need to explore the
efficacy of MStim treatment in previously dependent animals.
References


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Figure Legends

Figure 4.1 – Effects of MStim on VTA GABA neuron firing rate after reinstatement ethanol during withdrawal.

(A-C) Representative traces for GABA neuron response for (A) EtOH alone, (B) EtOH + MStim and (C) saline + MStim. (D) Baseline firing rate differences between the three groups. Note that EtOH alone maintained a higher baseline firing rate. (E) MStim blocks chronic EtOH-induced desensitization of GABA neurons to EtOH reinstatement. (F) Time course data with 50 sec bins demonstrating disparate effects among groups. Asterisks *, **, *** indicate significance levels $p<0.05$, $0.01$ and $0.001$, respectively.

Figure 4.2 – Basal dopamine release in the NAc following EtOH injection (2.5g/kg IP).

(A) Summarized time course of EtOH enhancement of basal DA release in the NAc. Note that naïve animals show distinct differences when compared to animal that received EtOH or MStim. (B) Comparison of [DA] at 100 min post-injection. (C) Comparison of [DA] at 120 min post-injection. Asterisks *, **, *** indicate significance levels $p<0.05$, $0.01$ and $0.001$, respectively.

Figure 4.3 – Blocking of EtOH-induced behavioral measures of withdrawal by MStim.

(A) Number of times the animal reared-up on hind legs in 30 min period. (B) Number of times the animal crossed through the middle third of the chamber in a 30 min period. (C) Subjective rating of tail-stiffness. (D) Subjective measure of the animal’s gait. Note that all measures improved with the concurrent administration of MStim during chronic EtOH exposure. (E-G) Representative traces of the animals movement patterns during testing. Asterisks *, **, *** indicate significance levels $p<0.05$, $0.01$ and $0.001$, respectively.

Figures
Figure 4.1
**Figure 4.2**

A. Graph showing the effect of Ethanol (2.5g/kg IP) on DA levels over time. The graph includes different treatment groups: Saline + MSlim, EtOH + MSlim, EtOH, and Naive.

B. Bar graph showing [DA] 100 MIN for EtOH, EtOH+MSlim, Sal+MSlim, and Naive conditions.

C. Bar graph showing [DA] 120 MIN for EtOH, EtOH+MSlim, Sal+MSlim, and Naive conditions.
Figure 4.3

A. REARING

B. OPEN-FIELD CROSSES

C. TAIL STIFFNESS

D. GAIT

OPEN-FIELD CROSSES

E. EtOH

F. EtOH + MStim

G. SAL + MStim
CHAPTER 5: Exercise Blocks Ethanol-Induced sensitization of Kappa Opioid Receptors

Exercise Blocks Ethanol-Induced sensitization of Kappa Opioid Receptors

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Running title: Exercise Blocks EtOH Changes to KORs

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Number of pages: 15
Number of figures: 3
Abstract: 120 words
Introduction: 496 words
Discussion: 412 words
Formatted for The Journal of Neuroscience
Abstract

Exercise has increasingly been utilized as an adjunctive treatment for alcohol-use disorder (AUD). This is in spite of sparse mechanistic understanding of neurologic effects influencing alcohol-induced substrate adaptations in the mesolimbic circuitry or elsewhere. These limitations blunt practitioner’s efficacy in developing evidence-based guidelines for exercise recommendations for AUD. Kappa opioid receptors (KORs) have been shown to increase sensitivity after chronic alcohol exposure. In this study we demonstrate that voluntary exercise alone decreases expression of KORs in the nucleus accumbens and the ventral tegmental area. These exercise-induced changes competitively alter chronic ethanol-induced changes in KOR expression in these brain regions. Curiously, we report that though voluntary exercises reduces ethanol seeking in chronically exposed mice, it potentiates drinking in saline exposed mice.
Introduction

It is estimated that over 28 million Americans are currently in need of treatment for alcohol abuse, resulting in over $249 billion in direct costs [1]. Making matters worse, only 13% of those needing intervention actually receive it. Thus, the economic, societal, familial, and personal costs associated with AUD are staggering.

Kappa Opioid Receptors
KORs are expressed extensively in the Nucleus accumbens (NAc), both in the core and the shell [2-4], where their activation inhibits DA release [2]. Data suggests that they are synthesized in the cell bodies of DA neurons in the ventral tegmental area (VTA) where they are expressed and also subsequently transported to terminals in the NAc where they are integrated into the presynaptic membrane [5]. Activation of kappa receptors is associated with dysphoria [6]. Evidence suggests that there is an upregulation of the kappa opioid system in alcohol dependent animals that may play a role in the increased seeking behavior seen with dependence [7]. This is demonstrated by a decrease in dependent-state seeking behavior when the KOR antagonist nor-BNI is administered while having no effect on non-dependent animals [8]. Further chronic intermittent ethanol exposure has been shown to increase the effect of KORs in the NAc. These data suggest a role for KORs in the synaptic adaptations that occur in dependence [6].

Exercise and the Mesolimbic Dopamine System
There is strong evidence that aerobic exercise is a beneficial adjunct to current pharmacological and psychological treatment protocols. Exercise has been shown to produce a series of changes
with relevance to the mesolimbic system. Aerobic exercise, similar to acute ethanol consumption, has been shown to increase levels of tyrosine hydroxylase, the rate limiting enzyme in DA synthesis, in the NAc [9, 10] (Macrae 1987). It has also been associated with burst activation of DA neurons in the VTA [11] (Wang and Tsien 2011). Further, 6-weeks of voluntary wheel running in rats increased D2 auto receptor density in the NAc [10]; a modification that has been associated with increased risk of addictive behavior [12-14]. However, exercise has been shown to increase D2R density in the dorsal striatum in a mouse model of Parkinson’s disease [15]. Though the majority of evidence suggests an ameliorative role for exercise [16, 17], there is intriguing evidence suggesting that excessive levels of exercise can potentiate addiction [18, 19]. Currently, the causes of these outcome discrepancies has not been shown. However, as there is very little consistency in methodology, type, intensity or duration of treatment protocols, disparate recommendations might be to blame. Evidence for opioid receptor changes with exercise is less concrete, appears to be highly region dependent [20], and is lacking in the mesolimbic system. To our knowledge, no one has directly measured changes in KORs in the ventral striatum in the context of exercise and ethanol. In this study we hypothesize that voluntary wheel-running will down-regulate KORs in the NAc. We further predict that exercise will block ethanol-induced sensitization of KORs and reduce alcohol consumption in chronically exposed mice.

**Material and Methods**

*Animals*
Male C57BL/6J and DBA/2J mice (Jackson Labs; aged 6-12 weeks) were given *ad libitum* access to food and water, and were maintained on a reverse 12:12-h light/dark cycle (lights on at 15:00 h). Mice were randomly assigned to one of three cohorts, ethanol without exercise, ethanol with exercise and saline with exercise. All mice were injected BID with ethanol (2.5g/kg; 16% w/v; IP) or an equivalent volume of saline for 14 days. Exercise groups were given *ad libitum* access to a running wheel. Intoxication was visually verified with loss of consciousness which decreased visually with dependence. All protocols and animal care procedures were in accordance with the National Institutes of Health Guide for the Care and Use of Laboratory Animals and approved by the Brigham Young University Institutional Animal Care and Use Committee. All efforts were made to minimize animal suffering and number of animals used in the present study.

**Brain Slice Preparation**

Isoflurane (Patterson Veterinary, Devens, MA) anesthetized mice were sacrificed by decapitation and brains were rapidly removed and transferred into ice-cold, pre-oxygenated (95% O2/5% CO2) artificial cerebral spinal fluid (aCSF) consisting of (in mM): NaCl (126), KCl (2.5), NaH2PO4 (1.2), CaCl2 (2.4), MgCl2 (1.2), NaHCO3 (25), glucose (11), L-ascorbic acid (0.4), pH adjusted to 7.4. Tissue was sectioned into 400 μm-thick coronal slices containing the striatum with a vibrating tissue slicer (Leica VT1000S, Vashaw Scientific, Norcross, GA). Brain slices were placed in a submersion recording chamber, and perfused at 1 ml/min at 32 °C with oxygenated aCSF.

**Fast Scan Cyclic Voltammetry**

Fast scan cyclic voltammetry (voltammetry) recordings of dopamine signals were performed and analyzed using Demon Voltammetry and Analysis Software [Demon Voltammetry and Analysis;
The carbon fiber electrode (7 μm X ~150 μm) potential was linearly scanned as a triangular waveform from -0.4 to 1.2 V and back to -0.4 V (Ag vs Ag/Cl) at a scan rate of 400 V/s. Cyclic voltammograms were recorded at the carbon fiber electrode every 100 msec by means of a potentiostat (Dagan Corporation, Minneapolis, MN). Dopamine release was evoked every 2 min through a bipolar stimulating electrode. For input/output experiments examining baseline dopamine signals across increasing current stimulations, single pulse baseline dopamine signals were collected (4 ms, 350 μA) until signals were stable for across 3 collections. Baseline single pulse responses were measured followed by concentration response for U50488 at 0.3 uM and 1 uM followed by a reversal dose of 1 uM nor-BNI; all drugs were bath applied. Each response was gathered from single-pulse stimulations given 2 min apart before introduction of the next drug concentration.

**Preparation of Brain Slices for Imaging and Confocal Microscopy**

Mice were anesthetized using isoflurane and underwent transcardial perfusion with 4% paraformaldehyde (PFA). Once perfused, brains were carefully removed and placed in 4% PFA for 24 hrs to facilitate continued fixation. After incubation in PFA, brains were placed in a solution of 30% sucrose in 1X PBS until the density of the brain matched that of the solution and the brains dropped to the bottom of the vial (~24-48 hrs). Brains were then flash frozen in dry ice and mounted on a cold microtome stage. Targeting the VTA and NAc, brains were sliced at 30 μm on the microtome and slices were placed in cryoprotectant (30% ethylene glycol, 30% sucrose, 0.00002% sodium azide, in 0.1 M PB) and kept at -20°C until staining. Slices were washed 3 times in 1x PBS for 10 minutes on a rotator. They were then blocked with a blocking buffer comprised of 4% normal goat serum, 0.1% Triton-X 100 and 1x PBS. Slices were then washed another 3
times in 0.2% PBST on a rotator. Primary antibodies were applied and allowed to incubate for 20 hours. Following staining the slices were washed 3 times in 0.2% PBST and secondary antibodies were applied. After a 2 hr incubation period they were washed another 3 times with 0.2% PBST and once with 1x PBS. Antibodies included Mouse anti-tyrosine hydroxylase (Novus, 1:1328), and Rabbit anti-KOR (LifeSpan, 1:200) as well as secondaries Alexa Fluor 405 Donkey Anti-Sheep from (1:900), Alexa Fluor 594 Goat anti-Rabbit (1:500). To mount slides, sections were placed on microscope slides and dried ~5 min. Once dried, a drop of vectashield (Vector Laboratories) was placed on the tissue, and a cover slip was placed on the slide. Slides set overnight, and then they were kept at 4°C until imaging. An Olympus FluoView FV1000 confocal microscope was used to image mounted slices. Brain slices were mounted on microscope slides and imaged under oil immersion at 40X. To ensure consistent readings between samples, a constant photomultiplier tube voltage and gain were set between all acquired images.

Statistical Analysis
For FSCV, evoked recordings were normalized to the established baseline within subjects and then averaged across subjects in corresponding time intervals. Comparisons were made using a Dunnett’s analysis. All statistical tests were performed in JMP13 (SAS, Cary, NC). Figures were compiled using IGOR Pro Software (Wavemetrics, Lake Oswego, OR).

For brain slice imaging, images were loaded into FIJI software. Images were duplicated to preserve the original settings while color thresholding and brightness contrast adjustments were made to determine the location of cells and create ROIs. ROIs were then projected back onto the unedited images where area and mean intensity were recorded for each channel. This process was
performed by three independent raters blinded to the hypothesis. To determine relative density of KORs, the ratio of mean fluorescence to area was determined.

**Results**

*KOR effects on Dopamine Release in the Context of Exercise and Ethanol*

Dopamine release was measured in each experimental group to measure changes in KOR activity with application of U50488, a KOR agonist and reversal with nor-BNI, a KOR antagonist. Significant differences were noted between the three groups at the 0.3 uM dose of U50488 ($F_{(2,12)} = 20.4619$, $p=0.0001$; **Fig. 5.1**). The ethanol no exercise group dropped to 81.4% (±4.1) of baseline while the ethanol with exercise group only dropped to 94.5% (±2.0). Conversely, the saline with exercise group increased evoked release to 108.3% (±4.2) (n=5 in all groups; $p=0.0228$ between Eth no Ex and Eth with Ex; $p<0.0001$ between Eth no Ex and Sal with Ex; $p=0.0166$ between Eth with Ex and Sal with Ex). When 1 uM U50488 was given the differences between groups increased significantly ($F_{(2,12)} = 22.9751$, $p<0.0001$). The ethanol no exercise group dropped to 70.1% (±2.1) of baseline and the ethanol with exercise dropped to 84.7% (±3.8). The saline with exercise remained generally unresponsive at 98.9% (±5.1) ($p=0.0127$ between Eth no Ex and Eth with Ex; $p<0.0001$ between Eth no Ex and Sal with Ex; $p=0.0150$ between Eth with Ex and Sal with Ex). Reversal with 1uM nor-BNI brought the ethanol no exercise, ethanol with exercise and saline with exercise groups back to 100.2% (±5.5), 92.0% (±4.5) and 99.7% (±4.0) respectively. There were no significant differences between these groups. This suggests that exercise desensitizes KORs and blunts ethanol-induced sensitization of the receptors.

*Immunohistochemical Analysis of KORs in the NAc and VTA*
Brain slices were acquired from each of the three groups in order to analyze expression patterns of KORs in the NAc and VTA. Following analysis, significant differences were noted in average MFI of KOR expressing cells in the NAc between the three groups ($F_{(2,3162)} = 353.7626, p<0.0001$; **Fig. 5.2A-C and G**). Average mean fluorescent intensity (MFI) of KOR expressing cells in the ethanol no exercise group was 7.08 (±0.085) while the ethanol with exercise group was 3.52 (±0.125). The saline with exercise group MFI was 3.77 (±0.11). Notably the ethanol with exercise group expressed an MFI similar to that of saline with exercise while both were significantly different from the ethanol no exercise group (n=6 animals per group with 6 slices analyzed per animal with multiple cells measured per slice; p<0.0001 between Eth no Ex and Eth with Ex; p<0.0001 between Eth no Ex and Sal with Ex; p=0.4787 between Eth with Ex and Sal with Ex). Expression patterns in the VTA followed the same trends as those in the NAc ($F_{(2,1766)} = 49.3301, p<0.0001$; **Fig. 5.2D-F and H**). The ethanol no exercise group was 5.46 (±0.15) and the MFI of the ethanol with exercise was 3.84 (±0.16). The saline with exercise remained closely tied to the other exercise group at 3.57 (±0.14) (n=same as in NAc; p<0.0001 between Eth no Ex and Eth with Ex; p<0.0001 between Eth no Ex and Sal with Ex; p=0.4046 between Eth with Ex and Sal with Ex). These findings indicate that exercise is sufficient to block ethanol-induced increased expression of KORs in both the NAc and the VTA.

**Effects of Exercise and Ethanol on Drink-in-the-Dark Behavior**

To assess exercise and ethanol effects on drinking behavior, drinking was measured on 4 consecutive days. Significant differences were noted between the composite average of all groups for all days ($F_{(2,43)} = 11.2596, p=0.0001$; **Fig. 5.3B**). The ethanol no exercise group drank on average 1.05g (±0.063) while the ethanol with exercise group drank 0.747g (±0.098).
Interestingly, the saline with exercise group drank more than either with an average consumption of 1.37g (±0.089) (Eth no Ex n=6, Eth and Ex n=3, Sal and Ex n=3; p=0.0323 between Eth no Ex and Eth with Ex; p=0.0124 between Eth no Ex and Sal with Ex; p<0.0001 between Eth with Ex and Sal with Ex). Ethanol consumption by day was significantly different only on days two and three. On day two the ethanol with exercise and saline with exercise groups averaged 0.672g (±0.16) and 1.51g (±0.13) respectively (p=0.009; Fig. 5.3A). On day three the ethanol with exercise and saline with exercise groups averaged 0.575g (±0.14) and 1.52g (±0.14) respectively (p=0.0035) while the ethanol no exercise group average 0.986g (±0.10) which was significantly different from the saline with exercise group (p=-0.0382; Fig. 5.3B) Exercise significantly reduces ethanol consumption in chronically exposed mice.

Discussion

In this study, KOR expression patterns were studied in the presence of ethanol and exercise to better understand the role of exercise in the natural reward pathways. Chronic ethanol exposure increases sensitivity of KORs while downregulating MORs and DORs in the NAc [22, 23]. We have shown that activation of peripheral mechanoreceptors, potentially similar to what occurs in consistent aerobic exercise, increases translocation of DORs to cellular membranes in the NAc potentially in opposition to what occurs in after chronic ethanol exposure. Mechanosensory input mediated through the dorsal column medial lemniscal pathway, provides collateral enervation, outside the canonical somatosensory pathways that terminate in the somatosensory cortex. These collaterals have been shown to alter neuron firing rate in the VTA [24] and influence neurotransmitter release and DOR expression in the NAc. In this context we can properly examine
the neurological effects of exercise in reference to their influence on the reward circuitry. Here we find that voluntary exercise alone is sufficient to produce a reduction in KOR sensitivity to U50488, a selective receptor agonist. It is important to note that mice in their natural habitat are accustomed to consistent daily exercise and it is possible that reduction in sensitivity and expression we report is actually the more normal state that a wild mouse would express and that the abnormally sedentary lifestyle of a laboratory mouse produces alterations in KOR expression due to lack of regular exercise. Regardless, it is evident that exercise directly influences the expression of KORs in both the VTA and NAc. Additionally, exercise is capable of blunting some of the increased expression of these receptors that normally accompanies chronic ethanol exposure.

We anticipated that because of these receptor changes that exercise would produce a reduction in drinking behavior in ethanol exposed but exercised mice and certainly in saline exposed and exercised mice. Indeed, exercise reduced drinking in chronically exposed mice. However, to our surprise, saline treated mice exposed to exercise exhibited increased drinking behavior. It has been reported that excessive levels of exercise carry the potential for dependence [18, 19] though no mechanistic explanations has been proven. The dichotomous findings suggesting both that exercise might be an effective adjunctive treatment for AUD while at the same time potentially increasing risk are unexplored. Further mechanistic investigations focusing on MORs and DORs in addition to KORs and the neurological circuits responsible for the mesolimbic effects of exercise are required to fully explain exercise’s potential as an adjunctive treatment modality.
References


**Figure Legends**

*Figure 5.1: Exercise blocks ethanol-induced sensitivity of KORs in the NAc*

Note that at concentrations of 0.03 uM U50488 and 1.0 uM U50488 there were significant differences between all groups. Asterisks *** indicate significance levels $p<0.001$, while ## indicates $p<0.01$.

*Figure 5.2: Exercise alters ethanol-induced KOR expression in the NAc and VTA*

(A-C) Representative images of KOR staining in the NAc demonstrating receptor expression differences, KORs are red. (D-F) Same as A-C but in the VTA. (G,H) Group MFI data in the NAc and VTA respectively, demonstrating that exercise decreases KOR expression in both brain regions. Asterisks *** indicate significance levels $p<0.001$

*Figure 5.3: Exercise decreases drinking in dependent but not naïve mice*

(A) Time course data demonstrating per day consumption between experimental groups. (B) Group showing composite drinking from all days. Note that all groups showed significant differences. Asterisks * and*** indicate significance levels $p<0.05$ and 0.001
Figures

Figure 5.1
Figure 5.2

KOR EXPRESSION

ETHANOL NO EXERCISE

ETHANOL EXERCISE

SALINE EXERCISE

NAc

VTA

NAc KOR MFI

VTA KOR MFI
Figure 5.3

A

DID ALCOHOL

- No EX Ethanol
- Ex Ethanol
- Ex Sal

B

EITOH CONSUMED (g)

- No Exercise Ethanol
- Exercise Ethanol
- Exercise Saline

* ** ***
CHAPTER 6: Discussion and Conclusions

Somatosensory Pathways Involved in Acupuncture-mediated Alterations to Mesolimbic Structures

For millennia, mechanistic explanations of acupuncture’s purported effects have centered on alterations to the balance of energy, or qi, meridians. These explanations have proven difficult to reconcile with modern neuroscientific investigative techniques and advances which have increasingly been used to explore the mechanistic underpinnings of an established body of positive outcome data. Acupuncture in the treatment of drug-use disorders has been an area of increasing western interest over the last decade. This interest has included hitherto unknown explanations of its neurological effects at the cellular level. Mechanoacupuncture (MA) at the HT7 acupoint, located medial to the flexor carpi ulnaris tendon at the wrist, has been shown to reduce VTA GABA neuron firing rate and decrease ethanol consumption (Yang et al., 2010). Further, the effects were shown to be mediated by delta opioid receptors (DORs) and initially driven by the dorsal column medial lemniscal pathway through the nucleus cuneatus, thalamus, and lateral habenula, not the spinothalamic tract, en route to altering firing rate in the VTA (Chang et al., 2017). This preliminary work set a foundational understanding essential to demystifying irrefutably positive outcome data that has been prejudicially discounted for generations in the West. Further, they provided a potentially unifying insight into common neurologically mechanistic explanation for the efficacy of manual therapeutics more generally; these include chiropractic medicine, physical therapy, etc…). More broadly we can refer to these disciplines as mechanoreceptor-based therapeutics. In light of these discoveries, this non-exhaustive body of work represents an attempt to further clarify, through mechanism and outcome, the potential of mechanoreceptor-based therapies to play a role in the treatment of drug-use disorders.
Mechanoreceptor Activation as the Primary Driver of Mesolimbic Alterations without Mechanoacupuncture

To determine the role of mechanoreceptors as the primary mediators of the mesolimbic responses noted, a novel technique was needed to selectively activate peripheral mechanoreceptors at a site distinct from HT7. We tested implantation of small vibrating motors next to the C7-T1 vertebrae, at the laminae (Chapter 2) as a means of providing direct stimulation to the DCML. These tests were successful in reducing VTA GABA neuron firing purely through mechanical stimulation (MStim), without MA. This method also represents a breakthrough in the studying of peripheral mechanoreceptor-based therapies. Previously, only direct mechanistic data from the peripheral nervous system or indirect measures of central nervous system effects had been reported.

Specificity of Effects relate to Mechanoreceptor Density and Type

Acupuncture stimulation at the wrist (HT7) or MStim at the cervical spine both represent areas of high mechanoreceptor density. In order to determine the importance of mechanoreceptors generally, we first tested the effects of MStim to an area relatively low in receptors density, the mid-thigh. We found that an 80 HZ (120 sec) MStim to the belly of the biceps femoris muscle was insufficient when compared to the effects noted by stimulation of the cervical spine at the same intensity and duration (Fig 3.2A).

Because different subtypes of mechanoreceptors respond to different frequencies of stimulation. Three frequencies were chosen to target specific mechanoreceptors and each was tested for 60 and 120 sec of stimulation. Of those chosen, 45 Hz enlists mostly Meissner’s corpuscles (Macefield, 2005; Fleming and Luo, 2013), while 115 Hz is more selective for Pacinian corpuscles (Zelena, 1978; Biswas et al., 2015). Both receptors are subcutaneously located. The frequency of 80 Hz lies between the two and likely activates both receptors. Additionally, all
three frequencies can activate Ruffini endings and Golgi tendon organs, two receptors that are morphologically similar to one another and are important as joint mechanoreceptors (Vega et al., 1996; Albuerne et al., 2000; Vega et al., 2009). The 50 and 80 Hz MStim produced a transient depression of GABA neurons in the VTA, with 80 Hz (120 sec) producing the largest and longest lasting effect. The 115 Hz stimulation failed to achieve VTA GABA neuron effects (Fig. 3.1). These data suggest that the effects of the MStim are likely mediated through Meissner’s corpuscles, Merkel cells and Ruffini endings rather than Pacinian corpuscles. Further simultaneous recordings from VTA DA neurons revealed that DA neuron firing increases, following MStim, transiently for an average of 500 sec. This time course is inversely mirrored by the described VTA GABA neuron depression. This is suggestive that the DA neuron firing is due to disinhibition from GABAergic input locally in the VTA. More experiments are required to fully determine the peripheral mechanoreceptors responsible for the described effects. One potential method of exploration could include the use of the ChR2-\textit{Venus} (ChR2V+) transgenic rat line for optogenetic stimulation studies (National BioResource Project). The ChR2V+ line uses the Thy 1.2 promotor to express the channelrhodopsin-2 (ChR2) transgene in myelinated dorsal root ganglion neurons (Tomita et al., 2009; Honjoh et al., 2014). This line has been shown to express ChR2 specifically in large diameter proprioceptive neurons, mainly Merkel Cells and Meissner’s corpuscles, rather than small diameter, nociceptive neurons (Ji et al., 2012). This is essential in the targeting of the DCML pathway and not the lateral spinothalamic tract. These neurons will then be selectively stimulated with transcutaneous light. To date, optogenetic stimulation has never been used to study mechanosensory modalities.

\textit{MStim Effects on NAc DA Levels are Locally Mediated by DORs and Acetylcholine Release}
Increased firing from VTA DA neurons, in the context of drug-abuse disorders, is most relevant if it translates to increase DA release in the NAc. We performed microdialysis experiments to measure changes in DA release following MStim. We anticipated that DA levels would demonstrate a sharp increase immediately following the treatment and then return to baseline. We were surprised to find that not only did MStim increase DA levels, the increase peaked at 60 min post-stimulation and didn’t return to baseline 120 min post-stimulation. These disparate effects in DA neuron firing and DA release were suggestive of two different etiologies. We found that MStim-induced increases in NAc DA levels can be blocked by antagonizing DORs in the NAc but not the VTA. Additionally, blockage of nicotinic and muscarinic acetylcholine receptors in the NAc also blocks DA increases (Fig. 3.6). Delta opioid receptors are located on local and projecting GABA neurons and cholinergic interneurons (CINs) in the NAc. Cholinergic interneuron activity increases DA release by activation of nicotinic receptors located on DA terminals. Activation of DORs in the NAc have been shown to increase DA and we show that MStim increases translocation of DOR to cell membranes in the NAc. Two theories could explain the DOR dependent increase of DA by MStim. First, increased release could be through disinhibition of CINs and DA terminals, both of which receive GABAergic input that is DOR dependent. Second, it is possible that direct activation of DORs on CINs could cause increased firing even though DORs are known to be \( G_i \) coupled GPCRs. This could occur through increased \( I_h \) or hyperpolarization currents which produce increased burst firing of CINs. To better isolate the role of disinhibition of DA terminals via GABA neuron inactivation versus increased \( I_h \) firing of CINs we could perform loose patch electrophysiological experiments on CINs in the presence of DPDPE, a DOR agonist in the genetically modified VGAT-CRE mouse strain. This strain marks VGAT expressing cells like GABA neurons with
CRE which would allow us to virally inactivate them without effecting the CINs. This would allow us to isolate the CINs and their specific responses to DOR activation and determine if burst firing occurs. Further, exploration with fast-scan cyclic voltammetry would allow us to measure evoked DA release response to DOR activation without the interference of DOR expressing GABA neurons. These experiments would allow us to more fully understand the interplay between DORs on CINs and those on GABA neurons in the MStim-induced DA increases.

**A Working Model of MStim Effects in the Mesolimbic Circuitry**

We developed a working model of a proposed mechanism by which MStim effects the VTA and NAc (Fig. 6.1). We propose that signals from peripheral mechanoreceptors are transduced through the DCML to the VPL thalamus. From there signals pass to the lateral habenula which sends glutamatergic projections to the NAc. Glutamate receptors on D2 expressing medium spiny neurons (D2 MSNs) increase their activity. These D2 MSNs release
met-Enkephalin, an endogenous ligand to the DOR. They also project back to the VTA via the indirect pathway and ultimately inhibit firing of local VTA GABA neurons, which results in a transient inhibition of VTA DA neuron firing. The importance of this NAc to VTA projection was verified by local lidocaine injection into the NAc; it blocked MStim-induced depression of VTA GABA neuron firing. Local NAc collaterals from D2 MSNs activate DORs on local GABA interneurons which cause CIN and DA terminal disinhibition; both of which result in increased DA release. Several important factors remain unknown in this process. The effects of mechanoacupuncture have been shown to be glutamate dependent in the NAc (Kim et al., 2018). The precise origin of these fibers is not known. This could be determined experimentally using dual single unit recording. One potential target for these studies is the rhomboid nucleus of the thalamus. It contains efferent projections that enervate the NAc and the other limbic structure (Vertes et al., 2006). These studies would provide direct evidence that neurons in the thalamus fire in tandem with neurons in the NAc or in the VTA.

**MStim Blockage of Markers of Chronic Ethanol Dependence**

Normally, a reinstatement dose of ethanol after 24 hours of withdrawal in the dependent animal will not cause a depression in VTA GABA neuron firing rate. This demonstrates the desensitization that occurs because a naïve animal will show a massive decrease in the presence of ethanol. Animals received MStim, via whole-body vibration at 80 HZ for 15 min BID, reacted to reinstatement ethanol in a manner that more closely resembles a saline treated animal (Chapter 5). Further, behavioral measures of dependence are largely mitigated with the addition of MStim to the process of dependence. Several possible explanations exist for this observed phenomenon. First, chronic ethanol has been shown to decrease DOR affinity in the NAc. We have shown that MStim significantly increases translocation of DORs to cellular membranes in
the NAc 2 hours post-MStim. These competing effects could be responsible for the protective influence of MStim over the normal adaptations resultant from chronic ethanol exposure. To further understand how MStim blocks measures of dependence after chronic ethanol exposure more study will be required. Evidence suggests that kappa opioid receptors (KORs) and mu opioid receptors (MORs) are important in chronic ethanol-induced mesolimbic adaptations with KORs increasing expression and MOR decreasing expression after chronic ethanol exposure. Both KORs and MORs need to be studied to determine if MStim alters their expression. Immunohistochemistry analysis of their expression patterns after MStim and colocalization with tyrosine hydroxylase and D2 receptors would help us isolate expression patterns on DA terminals, GABA neurons and CINs in the NAc.

**Exercise and Ethanol Dependence**

In chapter 5 we demonstrate that voluntary wheel running is sufficient to alter expression of KORs in the NAc and the VTA and their influence on evoked DA release in the NAc. These changes hold after chronic ethanol exposure. Further, ethanol drinking behavior was substantially reduced with exercise. Paradoxically, exercise without chronic ethanol increased drinking behavior even while decreasing expression of KORs, opposite to the effect elicited by chronic ethanol. It is noted that previous studies have reported conflicting results related to exercise as a treatment for drug-use disorders. Some reporting positively and some even showing potentiation of the condition (Ehringer et al., 2009; Berczik et al., 2012; Wang et al., 2014; Leasure et al., 2015). The direct connection between exercise and MStim is unknown. Interestingly, no one has ever published a direct mechanistic explanation of how exercise exerts its effects on the mesolimbic system. It remains unstudied whether these effects are mediated by cardiovascular means or in a more neurologically direct pathway similar to MStim. However,
logically, exercise activates mechanoreceptors. To date, no has reported real-time changes in neuron firing in connection with exercise. Such studies could be performed with an anesthetized rat whose head is sterotaxically stationary being placed on a treadmill. Natural reflexive responses would allow the rat to engage in treadmill running while electrophysiological measurements of neurons are taken. Additionally, these results could be compared to changes induced by passive motion of limbs versus pharmacological cardiovascular stress testing. Obviously, DOR and MOR changes with exercise would provide needed mechanistic understanding as well. Finally, intensity of exercise could be a major player in the explanation of disparate outcomes related to exercise as a treatment modality (Ni et al., 2012).

Conclusions and Future Directions

Mechanical stimulation holds great promise as an adjunctive treatment approach during acute medical detox, residential and outpatient addiction recovery programs. The non-pharmacological ability to alter GABA firing rate in the VTA and increase local DA release in the NAc is an astounding finding that warrants more exploration. Because of the high level of safety associated with this type of therapy, it hold the potential to provide a step forward in light of the low levels of efficacy of current treatment approaches. It creates the possibility to collaborations with alternative health-care providers including doctors of chiropractic, acupuncture and physical therapy. Future studies should continue to explore the mechanistic science behind MStim effects including, thalamic to NAc connections and the involvement of MORs and KORs. Future testing should also include testing in animals that have become dependent before MStim has been introduced to test its efficacy as a recovery modality. Obviously, translational studies in humans are required to test these effects in the human population. Optimal durations and frequency of treatments must to be explored to maximize
changes to the neuronal substrates discussed and to maximally alter behavioral outcomes. It is hoped that this work will lay a foundation to for a new treatment to improve outcomes for those struggling to overcome drug-use disorders.

References


Kyle Bills, DC, IDE, QME, MUA – *Curriculum Vitae*

**Education**

Brigham Young University  
*Ph.D. Candidate – Neuroscience*  
2016-2019

Parker University  
*DC - Doctor of Chiropractic*  
Summa Cum Laude  
Salutatorian  
2009

Brigham Young University  
*BS - Exercise Science*  
Magna Cum Laude  
2005

**Licensures**

State of California  
*License to practice Chiropractic*  
2009 – current

State of Utah  
*License to practice Chiropractic Medicine*  
2016 – current

State of California  
*Radiology operator and supervisor License*  
Licensed to perform diagnostic radiographs and supervise licensed radiology technicians  
2011 – current

**Publications**


**Abstracts**


**Presentations**
“Mechanoreceptor-based therapeutics and their role in the treating drug-use disorders” Parker University, Dallas TX (2019)

“Vibratory stimulation of cervical vertebrae modulates the discharge activity of ventral tegmental area neurons and dopamine release in the nucleus accumbens,” ACC-RAC Baltimore, MD (2019)


“Frequency dependent modulation of the mesolimbic system through peripheral mechanoreceptors,” Brigham Young University, (2018)

“Effects of Aerobic Exercise Intensity on Dopamine Release in the Nucleus Accumbens” Graduate Research Fair, Brigham Young University (2017)

“Changes in evoked dopamine release in the nucleus accumbens with moderate exercise” Grad Expo, Brigham Young University, Provo, UT (2017)

“Exercise induced down regulation of kappa opioid receptors in the nucleus accumbens” Grad Fad, Brigham Young University, Provo, UT (2017)

**External Funding**

PI: F32 PHS NIH NCCIH (AT009945)

PI: NCMIC Post-doctoral Fellowship
*Awarded to scholars the board believes can positively and substantially impact the future of chiropractic medicine through advances in research.* (2016-2020) Total 4 yrs = $20,000

PI: Activator Methods International
Research Equipment Grant – Activator V (2017) - $2000

**Internal Funding**

BYU Interdisciplinary Research Grant

Marjorie Hinckley Endowed Chair Award - $500
*Grant to present research at the Society for Neuroscience 2017, Washington DC*

Parker University
*President’s Scholarship* - $10,000
Highest scholarship awarded for academic attainment

Brigham Young University
*Half or Full Academic Scholarship*
All years of attendance

**Patents**

A device and method to induce interferential beat vibrations and frequencies into the body for treatment of pain, anxiety, depression, addiction, and sleep disorders

**Pedagogical Experience**
Teaching

Neuroscience 205 – Neurobiology  
Brigham Young University – Winter 2017, Spring 2018, Winter 2019  
Instructor of Record

Neuroscience 380 – Neuroanatomy  
Brigham Young University – Winter 2018  
Graduate Instructor

Physiology 363 – Advanced Physiology Lab  
Brigham Young University – Winter 2017  
Graduate Instructor

Courses Developed

Curriculum Redesign  
Neuroscience 205 – Neurobiology and Physiology 363 – Advanced Physiology Lab  
Brigham Young University

Functional Neurology in the Practice of Manual Medicine  
InnerCalm and Associates, course for continuing medical education credits. This is a web-based course I was asked to develop as a distance learning tool for practicing physicians.  
On-line Course Developer

Appointments

State of California  
Qualified Medical Evaluator (QME) appointment  
Designated to perform independent medical evaluations for the Department of Workers’ Compensation Medical Unit. Purpose is to provide substantial medical evidence pertaining to injured workers that can be used by workers’ compensation judges to determine outcomes.  
2011 - current

State of California  
Subject Matter Expert – Physical Medicine and Rehabilitation  
Ask to consult for the ongoing improvement of the State of California Qualified Medical Evaluator certification exam.  
2014 – current

Certifications and Boards

National Board of Chiropractic Examiners  
General practice of chiropractic  
2008 – Parts 1-4

National Board of Chiropractic Examiners  
Physiotherapy  
2008

Industrial Disability Evaluator (IDE) certification  
50 hours in the use of the American Medical Associations Guide to the Rating of Permanent Impairment. Extensive time given to medical legal report writing techniques.  
Dr. Jim Platto, DC, MPH

Manipulation Under Anesthesia (MUA)
Certification to perform manipulation assisted by general anesthesia.
Innercalm and Associates, Edward Cremata, DC, RN

Awards, Achievements, Associations

Ruth L. Kirchstein National Research Service Award
*NIH - NCCIH - Post-Doctoral Fellow (2019-2022)*

Research Presentation Award
*Oriental Medicine and Acupuncture (2018)*

Outstanding Research Presentation Award
*GS Society - 2017*

Parker University
*Academic awards for achievement in anatomy and biochemistry*
Top student in each series of classes

Parker University
*James W. Parker Philosophy Award*
“This award is given to one graduate, who, to an outstanding degree, has demonstrated the Parker principles of friendship, love of mankind, and the compassion to serve in the practice of chiropractic.” – Parker University

Parker University
*Salutatorian*

American Botanical Council
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Positions Held

Brigham Young University
*Post-Doctoral Fellow*
Department of Psychology and Neuroscience
Sept 2019

The Migraine and Neurological Rehabilitation Center
*Owner*
2018 - current

Brigham Young University
*Neuroscience Graduate Researcher*
Scott Steffensen Lab
Aug 2016 - 2019

Christopher Place Healthcare Review
*Medical Necessity Review Physician*
Sep 2016 – Present

State of California
*Subject Matter Expert – Physical Medicine and Rehabilitation*
2014 - present
Restoration Chiropractic
Owner
Aug 2012 - 2019

Restoration Chiropractic
Seminar Instructor
Spinal and Extremity Adjusting
for students from Life West and Palmer West Chiropractic Colleges
Jan 2010 – 2019

Dallas VA Medical Center
Intern/Resident
Examination and Treatment of Patients
2008 - 2009

Alexander Chiropractic
Treating Physician
Jan 2009 - Aug 2012

Parker University Health Clinics
Intern
Examination and Treatment of Patients
Jan 2007 - Jun 2008

Brigham Young University
Dr. Bruce Woolley, PharmD
Teaching Assistant
Anatomy, Physiology, and Pharmacology
Jan 2004 – Dec 2004

Brigham Young University
Laboratory of Dr. Bruce Woolley, PharmD
Research Assistant
Nutraceutical protocols to maximize bone density in women of child-bearing years
Jan 2004 – Dec 2004